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Moment-to-Moment Fluctuations in Neuronal Excitability Bias Subjective Perception Rather than Strategic Decision-Making

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Abstract

1
2 Perceiving an external stimulus not only depends on the physical features of the stimulus,
3 but also fundamentally on the current state of neuronal excitability, indexed by the power
4 of ongoing alpha-band and beta-band oscillations (8–30 Hz). Recent studies suggest that
5 heightened excitability does not improve perceptual acuity, but biases observers to report the
6 presence of a stimulus regardless of its physical presence. It is unknown whether this bias
7 is due to changes in observers' subjective perceptual experience (perceptual bias) or their
8 perception-independent decision-making strategy (decision bias). We tested these alternative
9 interpretations in an EEG experiment in which male and female human participants performed
10 two-interval forced choice (2IFC) detection and discrimination. According to signal detection
11 theory, perceptual bias only affects 2IFC detection, but not discrimination, while interval deci-
12 sion bias should be task-independent. We found that correct detection was more likely when
13 excitability before the stimulus-present interval exceeded that before the stimulus-absent inter-
14 val (i.e. 8–17 Hz power was weaker before the stimulus-present interval), consistent with an
15 effect of excitability on perceptual bias. By contrast, discrimination accuracy was unaffected
16 by excitability fluctuations between intervals, ruling out an effect on interval decision bias.
17 We conclude that the current state of neuronal excitability biases the perceptual experience
18 itself, rather than the decision process.

19 **Significance Statement:** The current state of neuronal excitability, indexed by the power
20 of ongoing low-frequency oscillations (8–30 Hz), has a strong influence on perception. How-
21 ever, the specific mechanism underlying this influence is a continuing subject of debate in
22 neuroscience. Previous research showed that states of heightened excitability make observers
23 report the presence of a sensory stimulus even when none is present. Heightened excitability
24 may therefore indicate a state of strategic decision-making (i.e. observers prefer to report
25 “Yes, I saw the stimulus”) or a state of amplified subjective perception (i.e. observers experi-
26 ence a stimulus even when none is present). Here, we tested these alternative interpretations
27 and found evidence that fluctuations in neuronal excitability bias the perceptual experience
28 itself, rather than the decision strategy.

29 Introduction

30 Ongoing neuronal activity just preceding, or in the absence of experimental events, is ubiq-
31 uitous in electrophysiological recordings in the form of “spontaneous” or “pre-stimulus” oscil-
32 lations. A prominent type of such spontaneous activity is the α - and β -rhythm (8–30 Hz),

33 which plays a key role in regulating cortical excitation and inhibition (Jensen and Mazaheri,
34 2010; Spitzer and Haegens, 2017). Specifically, states of weak α - and β -power (in addition to
35 other indices, such as specific α -phases) reflect increased excitability in sensory brain areas, as
36 indexed by the spike-firing rate (Haegens et al., 2011; Watson et al., 2018), multiunit activity
37 (van Kerkoerle et al., 2014), ongoing γ power (Spaak et al., 2012) and the hemodynamic fMRI
38 signal (Goldman et al., 2002; Becker et al., 2011).

39 How do spontaneous neural oscillations interact with the processing of sensory events? Numerous
40 studies have demonstrated that observers are more likely to detect visual targets that are preceded
41 by weak pre-stimulus low-frequency power (8–30 Hz), reflecting stronger neuronal excitability
42 (Ergenoglu et al., 2004; Chaumon and Busch, 2014). But does strong excitability help observers
43 distinguish more *accurately* between target and non-target stimuli, or does excitability simply make
44 all stimuli appear more target-like? Recent studies have demonstrated that in visual detection
45 tasks, strong excitability increases the hit rate in stimulus-present trials as well as the false alarm
46 rate in stimulus-absent trials (Limbach and Corballis, 2016; lemi et al., 2017). Moreover, recent
47 studies found that this effect is specific to tasks requiring the detection of target presence vs.
48 absence, while tasks requiring discrimination between two alternative target types are unaffected
49 by excitability (lemi et al., 2017; Samaha et al., 2017b). In sum, these findings indicate that
50 contrary to the previously dominant view in the literature (van Dijk et al., 2008; Romei et al.,
51 2008; Payne and Sekuler, 2014), heightened excitability does not lead to an increased perceptual
52 precision, but to a more liberal detection bias.

53 These findings could be regarded as evidence refuting an effect of excitability on perception
54 proper, showing instead an effect on observers' strategic *decision bias*: a deliberate preference to
55 report "yes, I saw the target" in both target-present and -absent trials. Accordingly, false alarms
56 induced by a decision bias during states of strong excitability are due to a shift in decision strategy.
57 However, not every change in bias implies a change in deliberate decision strategy (Witt et al.,
58 2015); alternatively, excitability might modulate *perceptual bias*: a change in the amplification of
59 the neural representation of both target and non-target stimuli. In tasks requiring the detection of
60 target presence vs. absence, this process boosts the perception of target presence in both target-
61 present and -absent trials. Accordingly, false alarms induced by perceptual bias during states
62 of strong excitability are due to genuine, albeit false, impressions of seeing a target. Evidently,
63 decision bias and perceptual bias each lead to very different theoretical interpretations of how

64 spontaneous brain activity is related to perception and behavior.

65 The present study was conducted in order to determine whether spontaneous fluctuations in
66 pre-stimulus low-frequency power (i.e. 5–30 Hz, a proxy for neuronal excitability) affect either
67 precision, perceptual bias or decision bias. To this end, we used a two-interval forced choice (2IFC)
68 paradigm, in which each trial includes a target and a non-target interval. In 2IFC detection, a
69 stimulus is presented in the target interval and no stimulus is presented in the non-target interval,
70 and observers report the interval comprising the stimulus. In 2IFC discrimination, a target-stimulus
71 (e.g. a left-tilted grating) is presented in one interval, and a non-target stimulus (e.g. a right-tilted
72 grating) in the other interval, and observers report the interval comprising the target.

73 We tested three models that represent alternative hypotheses on how weak pre-stimulus low-
74 frequency power, reflecting strong neuronal excitability, influence performance (see Methods for
75 details). If greater excitability improved perceptual *precision*, performance in both 2IFC de-
76 tection and discrimination should be most accurate when power in both intervals is weak. If
77 greater excitability leads to a more liberal *perceptual bias*, performance in 2IFC detection should
78 be most accurate when power is weak in the target-interval (enhancing correct impression of
79 stimulus-presence), but strong in the non-target interval (inhibiting false impression of stimulus
80 presence), implying that excitability during the stimulus-present interval exceeds excitability dur-
81 ing the stimulus-absent interval. Since this effect reflects a bias in the perception of stimulus
82 presence vs. absence, it should be specific to the detection task. If greater excitability leads to
83 a more liberal *decision bias*, performance in both 2IFC detection and 2IFC discrimination should
84 be most accurate when power is weak in the target-interval compared to the non-target interval,
85 indicating a strategic tendency to report the interval with the weakest power.

86 The results confirmed the predictions of the perceptual bias model, implying that spontaneous
87 fluctuations in excitability, indexed by α - and β -power, bias subjective perceptual experience rather
88 than strategic decision-making or precision.

89 **Materials and Methods**

90 **Participants**

91 Previous studies on the relationship between neuronal excitability and perception (Busch et al.,
92 2009; Lange et al., 2013; Chaumon and Busch, 2014; Iemi et al., 2017, e.g.) have typically re-
93 ported samples of 12–33 participants. To ensure a robust estimate of our neurophysiological
94 effect, we recruited a sample of 25 participants (mean: 29.3, SEM = 0.75 year old, 16 females, 2
95 left-handed). All participants had normal or corrected-to-normal vision and no history of neuro-
96 logical disorders. Each participant took part in two sessions, one for each task, on two separate
97 days within a 7-day period. One participant was excluded before EEG preprocessing and behav-
98 ioral analysis, because she could not participate in the second experiment. Two participants were
99 excluded after EEG preprocessing because of excessive artifacts. A total of 22 participants were
100 included in the analysis. Prior to the experiment, written informed consent was obtained from all
101 participants. All experimental procedures were approved by the ethics committee of the German
102 Psychological Society.

103 **Stimuli**

104 The experiment was written in MATLAB (RRID:SCR_001622) using the Psychophysics toolbox 3
105 (RRID:SCR_002881; Brainard, 1997; Pelli, 1997). Stimuli were presented on a black background,
106 using a gamma-linearized cathode ray tube monitor operated at 100 Hz and situated in a dark
107 room. Low-contrast Gabor patches tilted by 10° clockwise or counterclockwise from the vertical
108 meridian with a diameter of 0.75° visual angle were displayed at 10° to the left or to the right
109 (counterbalanced across conditions) of the fixation dot.

110 Each trial included two successive intervals, separated by a 2 s gap. Each interval lasted two frames
111 (0.02 s) and was indicated by a 50% reduction in the diameter of the fixation point (Figure 1).
112 A Gabor stimulus was presented in one or both intervals for a duration of two frames (0.02 s).
113 After a delay of 0.4 s following the second interval, the fixation dot turned into a question mark,
114 which instructed participants to deliver a response with their dominant hand via button-pressing,
115 in accordance with the task instructions. After the button press, the question mark disappeared
116 and participants received color-coded feedback: correct/incorrect responses were indicated by a

117 green/red fixation dot, lasting 0.2 s. After the feedback, the fixation dot turned white and a new
118 trial started.

119 For each participant and task, an adaptive staircase procedure (QUEST; Watson and Pelli, 1983)
120 was used to find the stimulus contrast yielding 75% accuracy. To ensure that the analysis included
121 only trials of similar contrast, we rejected outlier trials in which the difference between the pre-
122 sented contrast value and the final threshold estimated by QUEST exceeded $\pm 10\%$. Using this
123 procedure, we ensured that the 2IFC detection and discrimination tasks were equally difficult.

124 **Experimental Design**

125 Participants performed a 2IFC detection and a 2IFC discrimination task in two separate sessions.
126 Task order was counterbalanced across participants. Each session lasted approximately 1.5 h with
127 breaks and included 700 trials divided into 14 blocks of 50 trials each. For both tasks, each trial
128 included a target-interval and a non-target interval. The order of target and non-target intervals
129 within a trial was counterbalanced and randomized across trials, such that half of the trials were
130 target-first (T1) and non-target-first (nT1), respectively.

131 In the 2IFC detection task, a Gabor stimulus was presented in the target interval and a blank
132 screen was presented in the non-target interval (Figure 1a). Participants were informed that each
133 trial contained a stimulus, which could appear in either interval, and were instructed to report in
134 which interval they perceived the stimulus (“first” vs. “second”).

135 In the 2IFC discrimination task, each of the two intervals contained a Gabor stimulus: a left-tilted
136 Gabor appeared in the target interval and a right-tilted Gabor appeared in the non-target interval
137 (Figure 1c). Participants were informed that each trial contained two stimuli characterized by
138 different tilts, and were instructed to report in which interval they perceived the left-tilted target
139 (“first” vs. “second”).

140 **EEG recording and preprocessing**

141 EEG was recorded with a 64-channel Biosemi ActiveTwo system at a sampling rate of 1024 Hz.
142 Electrodes were placed according to the international 10-10 system (electrode locations can be
143 found on the Biosemi website: https://www.biosemi.com/download/Cap_coords_all.xls)

144 The horizontal and vertical electro-oculograms were recorded by additional electrodes at the lateral
145 canthi of both eyes and below the eyes, respectively.

146 The EEGLAB toolbox version 11, running on MATLAB (R2010b), was used to process and analyze
147 the data (Delorme, 2004). Data were re-referenced to the average of all electrodes, epoched from
148 -3.7 to 0.7 s relative to the second interval onset and down-sampled to 256 Hz. The data were
149 then filtered using an acausal band-pass filter between 0.25 and 80 Hz. Gross artifacts (eye blinks,
150 and noisy data segments) were removed manually, and entire trials were discarded when a blink
151 occurred within a critical 0.5 s time window preceding interval onset, to ensure that participants'
152 eyes were open at interval onset. After rejecting trials with EEG artifacts and contrast outliers,
153 the total number of trials analyzed was 680 (5.5 SEM) and 645 (10.5 SEM) for the detection and
154 discrimination session, respectively.

155 Noisy channels were selected manually on a trial-by-trial basis for spherical spline interpolation
156 (Perrin et al., 1989). In the detection task we interpolated on average 8.1 channels (SEM = 1.13)
157 in 22.3 trials (SEM = 4.74) in 21 out of 22 participants. In the discrimination task we interpolated
158 on average 8.5 channels (SEM = 0.85) in 21.7 trials (SEM = 3.71) in 19 out of 22 participants.
159 Furthermore, the EEG data were transformed using independent component analysis (ICA), and
160 SASICA (Chaumon et al., 2015) was used to guide the exclusion of IC related to noisy channels
161 and muscular contractions, as well as blinks and eye movements occurring before or after the
162 critical intervals.

163 We then re-epoched the trials relative to the onsets of target and non-target interval of each
164 trial, enabling us to analyze within-trial, between-interval fluctuations in oscillatory power. Time-
165 frequency analysis was carried out using a wavelet transform (Morlet wavelets, 30 frequencies,
166 frequency range: 1–30 Hz, number of cycles increasing linearly from 1 to 12). Thus, a wavelet
167 at 10 Hz was 4.4 cycles long and had a temporal resolution σ_t of 0.14 s and a spectral resolution
168 σ_f of 4.53 Hz. Since wavelet analysis is computed by convolving the data with a function that
169 is extended in time, it is possible that pre-stimulus effects close to stimulus onset are actually
170 affected by post-stimulus data. Iemi et al. (2017) determined the extent of this contamination by
171 estimating the wavelet's temporal resolution σ_t (Tallon-Baudry et al., 1996). Thus, we consider
172 effects as truly "pre-stimulus", only if they occur at time points earlier than interval onset - σ_t
173 (indicated with a red line in Figure2a/c, 3a/e, 4a/d/f/h).

174 **Modeling the relationship between oscillatory power and behavioral performance**

175 **Signal Detection Models**

176 Signal detection theory (Macmillan and Creelman, 2005, Figure 1b/c) provides an account of
177 behavioral performance and perceptual decision making in 2IFC detection and discrimination
178 tasks.

179 For a 2IFC detection task (Figure 1a), SDT posits that observers sample an internal response
180 in each interval, compare the two internal responses, and report whichever interval yielded the
181 stronger response. Thus, if the internal response during the target (stimulus-present) interval
182 exceeds the response during the non-target (stimulus-absent) interval, the participant makes
183 a correct detection. Across trials, overall accuracy in 2IFC detection depends on the relative
184 distance between the response distributions for stimulus-present and stimulus-absent intervals
185 (the two-dimensional Gaussian distributions in Figure 1b).

186 For a 2IFC discrimination task (Figure 1c), SDT posits that in each interval, observers sample
187 the internal responses of two feature detectors selective for the target and non-target stimulus,
188 respectively. The relative strength of these two responses serves as an index of evidence of target-
189 presence in a given interval. Observers compare this evidence between both intervals and report
190 whichever interval yielded the strongest evidence (Figure 1d). If the strength of evidence for
191 target-presence in the target-interval exceeds the strength of evidence in the non-target interval,
192 the participant makes a correct response. Across trials, overall accuracy in 2IFC discrimination
193 depends on the relative distance between the response distributions for target and non-target
194 intervals (two-dimensional Gaussian distributions in Figure 1d). Note that 2IFC detection is
195 based on comparing the responses of a single signal detector across two intervals, while 2IFC
196 discrimination is based on comparing the relative strength of two feature detectors across two
197 intervals.

198 As described in the Introduction, different models hypothesize that pre-stimulus low-frequency
199 power (i.e. 5–30 Hz, a proxy for neuronal excitability) affects either perceptual accuracy, percep-
200 tual bias, or decision bias. Importantly, these models make specific, testable predictions regarding
201 the relationship between pre-stimulus power and performance in 2IFC detection and discrimination
202 tasks.

203 According to the precision model, weak pre-stimulus power (i.e. greater excitability) improves the
204 accuracy in perceptual tasks by increasing the relative distance between the response distributions
205 in the target and non-target intervals, possibly via reduction of the trial-by-trial response variability
206 (lemi et al., 2017). In 2IFC detection stronger excitability results in a greater distance between the
207 response distributions of stimulus-present and -absent intervals. In 2IFC discrimination stronger
208 excitability results in a greater difference in target evidence between target and non-target intervals.
209 Thus, the precision model predicts that greater accuracy is related to weaker overall power in both
210 the target and the non-target interval in both detection and discrimination.

211 According to the perceptual bias model, weak pre-stimulus power (i.e. greater excitability), am-
212 plifies internal responses to any kind of stimulus. In 2IFC detection, such an amplification would
213 improve accuracy if amplification happened to be stronger in the stimulus-present compared to
214 the stimulus-absent interval, thus increasing the relative distance between the internal responses
215 in target and non-target intervals (Figure 1b). In other words, 2IFC detection accuracy should be
216 influenced by the balance of excitability and inhibition between the stimulus-present and stimulus-
217 absent interval. In 2IFC discrimination, stronger amplification in either target or non-target
218 interval would simultaneously increase internal responses of both target and non-target feature
219 detectors in that interval, leaving the relative distance between their response distributions (i.e.
220 target evidence) unchanged (Figure 1d). In sum, the perceptual bias model predicts that 2IFC
221 detection accuracy is greater when pre-stimulus power is weaker in the stimulus-present interval
222 compared to the stimulus-absent interval, while 2IFC discrimination accuracy is expected to be
223 unaffected by between-interval fluctuations of pre-stimulus power.

224 [Figure 1 about here.]

225 According to the decision bias model, weak pre-stimulus power influences observers' strategic deci-
226 sion making, rather than their perception, by increasing their tendency to report the interval with
227 weakest power (i.e. strongest excitability). Importantly, this tendency should be task-independent.
228 For 2IFC detection, this interval bias improves accuracy if pre-stimulus power is weaker in the
229 stimulus-present compared to the stimulus-absent interval (similar to a perceptual bias). Likewise,
230 interval bias improves 2IFC discrimination accuracy if pre-stimulus power is weaker in the target
231 interval compared to the non-target interval. Thus, in contrast to the perceptual bias model,
232 the decision bias model predicts that *both* 2IFC detection and 2IFC discrimination accuracy is

233 greater when pre-stimulus power is weaker in the stimulus-present/target interval compared to
234 the stimulus-absent/non-target interval, respectively.

235 **Statistical analysis**

236 The analysis included oscillatory power at all electrodes, at frequencies between 5 and 30 Hz and
237 between -0.5 and 0 s relative to interval onset.

238 **Generalized linear modeling** The predictions of the precision model concern the *overall* oscil-
239 latory power in the two intervals within a trial. Thus, for each single trial, time point, frequency,
240 and electrode, we computed a measure, P_{ave} , reflecting power averaged across the two intervals
241 within a trial.

242 The predictions of the perceptual bias and decision bias models concern the *relative* oscillatory
243 power between the two intervals within a trial. Thus, for each single trial, time point, frequency,
244 and electrode, we computed a measure, P_{rel} , comparing oscillatory power between the two inter-
245 vals as:

$$P_{rel} = \frac{P_T}{P_{nT}} \quad (1)$$

246 where P_T is power in the stimulus-present interval in 2IFC detection, and target interval in 2IFC
247 discrimination and P_{nT} is power in the stimulus-absent interval in 2IFC detection and the non-
248 target interval in 2IFC discrimination. Thus, $P_{rel} > 1$ indicates that power was relatively stronger
249 in the to-be-reported interval. P_{rel} and P_{ave} were rank-scored to mitigate the influence of extreme
250 values.

251 Next, we modeled the relationship between single-trial oscillatory power and response accuracy and
252 interval order using multilevel generalized linear modeling (GLM) (Cohen and Cavanagh, 2011;
253 Samaha et al., 2017b). Including interval order as a regressor enabled us to remove any possi-
254 ble contribution of the interval order from the estimation of the accuracy predictor. For each
255 participant and for each electrode, frequency, and time point, we fit a regression model of the
256 form:

$$X = \beta_0 + \beta_1 A + \beta_2 O + \varepsilon \quad (2)$$

257 where X is a continuous measure of oscillatory power (i.e. P_{ave} for the precision model and P_{rel}
258 for the bias models), A the accuracy (correct/incorrect) coded as a 1/-1 variable, O the interval
259 order (target first or non-target first) coded as a 1/-1 variable, β_0 , β_1 , and β_2 the estimated
260 coefficients, and ε the residual error. This GLM corresponds to a linear regression model, where
261 the coefficients β_1 and β_2 represent the independent contributions of the accuracy and the interval
262 order predictors, respectively, in explaining the observed power (P_{rel} or P_{ave}). GLMs were fit
263 separately for detection and discrimination tasks.

264 **Statistical testing and effect size** We then tested whether the regression coefficients β_1 and
265 β_2 at each electrode, frequency, and time point were significantly different from zero within
266 participants, and consistent across the sample of participants, using separate statistical tests at
267 the participant level and at the group level. Again, this procedure was carried out separately for
268 the 2IFC detection and 2IFC discrimination task.

269 At the participant level, we permuted the mapping between single trial power and single trial
270 accuracy/interval order 1000 times, recomputing the beta coefficients each time. This procedure
271 creates a within-participant null hypothesis distribution of the β coefficients. The β coefficients
272 associated with the true data mapping were then converted to a z-statistic relative to the mean
273 and standard deviation of the distribution of the permuted data, resulting in a z-score for each
274 participant and time-frequency-electrode point.

275 At the group level, we then tested whether z-scores of the β_1 and β_2 coefficients were significant
276 across participants (i.e. whether their signs were consistent) using a non-parametric cluster based
277 permutation test, which also addresses multiple comparisons across time points, frequencies and
278 electrodes (Maris and Oostenveld, 2007). We obtained a distribution of z-scores under the null
279 hypothesis by randomly permuting their signs 5000 times. On each iteration, we tested the
280 resulting z-scores with a two-tailed t-test against zero and assessed the sum of the t-values within
281 largest contiguous cluster of significant time-frequency-electrode points (cluster p-value = 0.01),
282 resulting in a distribution of t-sums expected under the null hypothesis. A final p-value was
283 calculated as the proportion of t-sums under the null hypothesis larger than the sum of t-values

284 within clusters in the observed data. Thus, p-values smaller than 0.01 indicate that the observed
285 β coefficients were significantly different from zero (two-sided).

286 We computed Cohen's d to estimate the effect size of significant clusters of interest. For each
287 time-frequency-electrode point of the significant cluster, Cohen's d was estimated by dividing the
288 t-statistics by the square root of the number of participants. Conventionally, Cohen's d indicates
289 whether the effect size is small (if $d < 0.2$), medium (if $0.2 < d < 0.8$) or large (if $d > 0.8$)
290 (Cohen, 1988; Lakens, 2013).

291 **Bayes factor analysis** The perceptual bias model predicts a relationship between P_{rel} and
292 accuracy in 2IFC detection, but a null effect in 2IFC discrimination. However, in conventional
293 inferential statistics, a non-significant result only indicates that the null hypothesis cannot be
294 rejected. It does not necessarily follow that the null hypothesis is actually true; it is possible that
295 the data might be inconclusive, e.g. due to insufficient statistical power. Thus, to directly estimate
296 evidence supporting the null hypothesis, we estimated the JZS Bayes factor (BF; Jeffreys, 1961;
297 Zellner and Siow, 1980; Rouder et al., 2009). The JZS BF is a Bayesian measures of evidence
298 which takes the form of an odds ratio: i.e. the probability of the data under H_1 relative to
299 that under H_0 . Conventionally, BF indicates whether there is evidence supporting the alternative
300 hypothesis ($H_1: \beta \neq 0$) if $BF > 3$, or supporting the null hypothesis ($H_0: \beta = 0$) if
301 $BF < 1/3$, or whether the evidence is inconclusive (if $1/3 < BF < 3$). For example,
302 a Bayes factor of $BF = 1/3$ indicates that the data are three times more likely under the H_0
303 than under the H_1 . For the significant negative t-statistics, found by the cluster test, we set the
304 prior on effect size following a Cauchy distribution with a scale factor 0.707, as recommended by
305 Rouder et al. (2009). We then computed for each time point the proportion of cluster electrodes
306 and frequencies yielding evidence for H_1 and H_0 , respectively (see insets below the time-frequency
307 plots in Figure 2a/c, 3e).

308 **Results**

309 **Behavior**

310 For each participant, an adaptive staircase procedure (see *Methods*) adjusted stimulus contrast
311 to ensure a proportion of 75% correct responses in both the 2IFC detection and the discrimina-

312 tion task. The participants included in the analysis had a mean proportion of correct detection
313 responses of 73.2 % (SEM = 0.002) and a mean proportion of correct discrimination responses
314 of 72.5 % (SEM = 0.007), indicating that the staircase procedure was successful. On average,
315 the stimulus contrast necessary for achieving this level of performance was higher in the 2IFC
316 discrimination task than in the 2IFC detection task (two-tailed paired-sample t test: $t(21) = 5.77$,
317 $p < 0.001$), which is consistent with previous work (lemi et al., 2017). The group-average con-
318 trast was 7.2% (SEM = 0.2) and 41.6% (SEM = 6.1) in the detection and discrimination task,
319 respectively.

320 EEG

321 This study aimed to test three models of the relationship between low-frequency oscillatory power
322 as a measure of excitability and performance in 2IFC detection and discrimination. To recap,
323 the precision model predicts that correct responses are associated with weak overall pre-stimulus
324 power in both intervals (i.e. low P_{ave}). The perceptual bias model predicts that correct responses
325 are associated with relatively weaker pre-stimulus power in the target interval compared to the
326 non-target interval (i.e. low P_{rel}), but only in the detection task. The decision bias model predicts
327 this association for both the detection and discrimination task (see Methods for details).

328 To test these models, we analyzed both tasks using GLM to model within each participant the
329 contributions of response accuracy (β_1 regressor) and interval order (β_2 regressor; target-first
330 vs. non-target first) on either P_{ave} (i.e. overall power averaged across the two intervals; to
331 test the precision model), or on P_{rel} (i.e. power in the target interval relative to the power in
332 the non-target interval; to test the perceptual bias and decision bias models). We then used a
333 cluster permutation test to determine whether regressors were significantly different from 0 across
334 participants.

335 **Precision Model** The group-level statistical test of β_1 (accuracy) identified significant clusters
336 in neither 2IFC detection nor discrimination. In other words, 2IFC accuracy did not correlate with
337 P_{ave} across participants. To provide evidence of a true null effect of accuracy on P_{ave} , as opposed
338 to merely inconclusive evidence, we used Bayes Factor (BF) analysis to quantify the proportion of
339 data points providing evidence of an effect (H_1) or evidence of a null effect (H_0). We restricted
340 this analysis to the significant time-frequency-electrode cluster found for β_1 in the bias model for

341 2IFC detection (see below, Figure 3a). The BF analysis revealed that for both 2IFC detection
342 and discrimination, the proportion of data points in favor of a null effect by far outnumbered the
343 proportion of data points in favor of an effect ($H_0 > H_1$, bottom insets of Figure 2a/c). In sum,
344 the relationship between P_{ave} and 2IFC detection and discrimination accuracy was not merely
345 weak or inconclusive, but entirely absent. These findings reject the precision model.

346 The group-level statistical test of β_2 (interval order) identified a significant effect of interval
347 order for 2IFC detection (p-value = 0.003), starting from -0.5 s relative to interval onset and at
348 frequencies between 7 and 24 Hz with an occipital topography (Figure 4a/b). In other words,
349 pre-stimulus 7–24 Hz P_{ave} was greater in trials when a stimulus was presented in the first interval
350 (target-first: T1) relative to trials when it was presented in the second interval (non-target-first:
351 nT1; Figure 4c). By contrast, no significant clusters were found for β_2 in 2IFC discrimination
352 (see Figure 4d/e).

353 [Figure 2 about here.]

354 **Perceptual and Decision Bias Model** The group-level statistical test of β_1 (accuracy) in the
355 2IFC detection task yielded a significant negative cluster (p-value = 0.005) starting from -0.344 s
356 before interval onset and at frequencies between 8 and 17 Hz (Figure 3a). In other words, correct
357 detection was associated on a trial-by-trial basis with lower 8–17 Hz P_{rel} , i.e. reduced α - and
358 β -power in the time window before the stimulus-present interval relative to the stimulus-absent
359 interval (Figure 3b). The topography of this negative effect evolved from fronto-central to parieto-
360 occipital electrodes (Figure 3c). The peak of this cluster was at electrode FC4, at 13 Hz and at
361 -0.305 s before interval onset ($t(21) = -5.20$). Cohen's d estimated within this significant cluster
362 had a median of -0.290, indicating a medium effect size (Figure 3d). Note that this effect in 2IFC
363 detection is predicted by both the perceptual bias and the decision bias model.

364 No significant clusters were found for β_1 in the 2IFC discrimination task (Figure 3e). In other
365 words, discrimination accuracy did not correlate with differences in P_{rel} (Figure 3f). We then
366 tested whether there was evidence of a true null effect of accuracy on P_{rel} , using BF analysis as
367 described above. We restricted this analysis to the significant time-frequency-electrode cluster
368 found for β_1 in 2IFC detection (Figure 3a). The BF analysis revealed that the proportion of data
369 points in favor of a null effect on 2IFC discrimination accuracy by far outnumbered the proportion

370 of data points in favor of an effect ($H_0 > H_1$, bottom insets of Figure 3e). Hence, the
371 relationship between 2IFC discrimination accuracy and P_{rel} was not merely weak or inconclusive,
372 but entirely absent. In sum, the results confirm the prediction of the perceptual bias model that
373 for 2IFC detection, but not 2IFC discrimination, relatively weak power before the target interval
374 and strong power before the non-target interval is related to higher accuracy.

375 [Figure 3 about here.]

376 The group-level statistical test of β_2 (trial order) found significant clusters in neither 2IFC detection
377 (Figure 4f/g) nor discrimination (Figure 4h/i).

378 [Figure 4 about here.]

379 Discussion

380 Excitability modulates perceptual bias rather than decision bias

381 What are the perceptual consequences of spontaneous fluctuations in neuronal excitability? Ac-
382 cumulating evidence suggests that, during states of strong neuronal excitability, indexed by weak
383 ongoing α - and β -power, observers are more likely to report the presence of a sensory target,
384 irrespective of its actual physical presence. Thus, contrary to the previously dominant view (e.g.
385 Ergenoglu et al., 2004; Payne and Sekuler, 2014), strong excitability reflects a state of liberal
386 detection criterion/bias rather than of improved perceptual acuity/sensitivity. What is the mecha-
387 nism linking fluctuations of excitability and bias? According to SDT, two alternative mechanisms
388 are possible. On the one hand, strong excitability could indicate a state of more permissive de-
389 tection strategy, during which observers prefer to report “yes, I saw the target”. This mechanism
390 is referred to as *decision bias*. On the other hand, strong excitability could reflect a state of in-
391 creased baseline sensory processing, resulting in an amplification of the neural responses to both
392 target and non-target stimuli. At the behavioral level, this is paralleled by an amplification of
393 subjective perceptual experience, during which observers “perceive” the presence of a target even
394 when it is not physically present. This mechanism is referred to as *perceptual bias*. Past studies
395 using single-interval detection tasks (Jemi et al., 2017; Limbach and Corballis, 2016) were unable

396 to distinguish between these alternative interpretations of excitability, because standard SDT
397 analysis cannot determine the underlying source of the bias, be it perceptual or decision-based
398 (Wixted and Stretch, 2000; Witt et al., 2015).

399 In this study, we addressed the issue by analyzing the relationship between low-frequency oscillatory
400 power (5–30 Hz), as a measure of neuronal excitability, and performance in 2IFC detection and
401 discrimination tasks, which are differently affected by perceptual bias and decision bias. The
402 predictions of a SDT model of perceptual bias are twofold. First, 2IFC detections should be
403 most accurate when excitability in the stimulus-present interval exceeds that in the stimulus-
404 absent interval, reflecting an amplification of the stimulus representation in the stimulus-present
405 interval and a dampening of the representation in the stimulus absent interval. Second, in 2IFC
406 discrimination, fluctuations of excitability between target and non-target intervals should not
407 affect discrimination accuracy. This is because a change in global excitability (i.e. not specific
408 to a certain feature value) affects the response of all feature detectors equally, without changing
409 their relative strength, which determines the evidence for target presence. By contrast, a SDT
410 model of decision bias posits that fluctuations in excitability influence the observer’s strategic
411 decision behavior, rather than perceptual processing. Note that a “yes”-bias, as in a single-
412 interval detection task, cannot affect decisions in a 2IFC detection task, because “yes, I saw it” is
413 not among the given options. However, an interval decision bias predicts a tendency to report the
414 interval with stronger excitability, regardless of perceptual task, and should therefore be manifest
415 in both 2IFC detection and 2IFC discrimination.

416 To test these alternative models, we analyzed how 2IFC detection and discrimination accuracy is re-
417 lated to excitability in target and non-target intervals (P_{rel}). We found that detection was most ac-
418 curate when pre-stimulus α - and β -power was lower before the stimulus-present interval relative to
419 the stimulus-absent interval (i.e. low P_{rel}). This effect rules out a “yes”-decision-bias that might
420 have affected previous findings from single-interval detection tasks (e.g. Chaumon and Busch,
421 2014; Limbach and Corballis, 2016; lemi et al., 2017). Moreover, using Bayes factor analysis we
422 found evidence that discrimination accuracy was unaffected by between-interval fluctuations of ex-
423 citability, ruling out an interval decision bias model. Taken together, the effect on 2IFC detection
424 and the evidence of a null effect on 2IFC discrimination confirm the predictions of the perceptual
425 bias model.

426 **Excitability does not affect perceptual acuity**

427 It is important to note that the effect of perceptual bias on 2IFC detection, i.e. when excitability
428 is specifically strong (i.e. weak low-frequency power) in the stimulus-present interval, merely
429 represents a serendipitous distortion of subjective perception “in the right direction” rather than
430 an actual improvement in perceptual acuity. By contrast, the precision model predicts that overall
431 excitability in both intervals improves detection and discrimination accuracy. However, using
432 Bayes factor analysis we found that overall excitability (P_{ave}) affected neither 2IFC detection
433 nor discrimination accuracy (Figure 2a). This result replicates, in a 2IFC paradigm, the findings
434 of three recent studies, reporting a null effect of excitability on single interval yes/no detection
435 sensitivity (Limbach and Corballis, 2016; lemi et al., 2017) and 2AFC discrimination accuracy
436 (lemi et al., 2017; Samaha et al., 2017b). Taken together, these findings challenge the long-held
437 notion that neuronal excitability affects the accuracy of perceptual decisions (van Dijk et al., 2008;
438 Romei et al., 2008; Payne and Sekuler, 2014). This notion has been based on the observation
439 that successful stimulus detection (hit-rate) is associated with relatively stronger excitability. Such
440 findings have been obtained with visual (Ergenoglu et al., 2004; van Dijk et al., 2008), auditory
441 (Leske et al., 2015) and somatosensory detection (Baumgarten et al., 2016) and for detection of
442 TMS-induced phosphenes (Romei et al., 2008; Samaha et al., 2017a). However, without testing
443 for an effect on the false-alarm rate on stimulus-absent trials, it is possible that excitability affects
444 rather the bias to report a stimulus, irrespective of whether or not this is accurate. Indeed, recent
445 studies analyzing signal detection measures found that increased excitability is associated with
446 a more liberal detection bias in both vision (Limbach and Corballis, 2016; lemi et al., 2017) and
447 somatosensation (Craddock et al., 2017). Our results are also consistent with several experiments
448 that found no effect of excitability on multiple-alternative-forced-choice (mAFC) *discrimination*
449 performance (e.g. Bays et al., 2015; see lemi et al., 2017 for a comprehensive literature review).
450 A SDT model of perceptual bias, in fact, predicts these null findings because discrimination
451 performance in mAFC tasks is unaffected by a “yes”-bias, and a modulation of excitability does
452 not change the discriminability between response alternatives (lemi et al., 2017).

453 Accumulating evidence suggests that spontaneous neural oscillations modulate subjective, rather
454 than objective, measures of performance in perceptual tasks. While replicating the finding that
455 states of heightened excitability do not improve objective perceptual accuracy, two recent studies
456 additionally demonstrated that excitability instead biases observers to report higher confidence in

457 2AFC discrimination (Samaha et al., 2017b) and higher visibility ratings (Benwell et al., 2017).
458 These results can be reconciled by a SDT model of perceptual bias. For example, in a 2AFC
459 discrimination task, confidence, unlike accuracy, is thought to depend on the absolute amount of
460 evidence in favor of the chosen stimulus alternative, regardless of the amount of evidence against
461 this choice (Zylberberg et al., 2012; Maniscalco et al., 2016). According to a perceptual bias
462 model, heightened excitability amplifies evidence for both stimulus alternatives simultaneously
463 (Iemi et al., 2017). Thereby, a perceptual bias amplifies evidence for the chosen alternative and,
464 in turn, amplifies subjective confidence and subjective visibility, while leaving objective accuracy
465 unchanged. Taken together, these results provide suggestive evidence for the perceptual bias
466 model.

467 **Spectral and topographical characteristics of the experimental effects.**

468 Correct detection was more likely when low-frequency power before the stimulus-present inter-
469 val was weaker relative to the stimulus-absent interval (Figure 3a–c). The effect of between-
470 interval power fluctuations on detection accuracy was widely distributed over many electrodes
471 and spanned frequencies between 7-18 Hz. The topography of this effect evolved from a fronto-
472 central to parieto-occipital topography (Figure 3c). This pattern is consistent with previous
473 studies using single-interval perceptual tasks reporting either a fronto-central (Busch et al., 2009;
474 Achim et al., 2013), parieto-occipital (Ergenoglu et al., 2004; van Dijk et al., 2008; Romei et al.,
475 2008; Lange et al., 2013; Chaumon and Busch, 2014; Mathewson et al., 2014; Samaha et al.,
476 2017b), or widespread topography (Iemi et al., 2017; Benwell et al., 2017). Furthermore, the
477 broad frequency range of this effect (Figure 3a) is consistent with recent reports (Iemi et al.,
478 2017; Samaha et al., 2017b; Benwell et al., 2017) and is in line with studies showing that α - and
479 β -oscillations are typically comodulated in time and colocalized in space (Bastos et al., 2015;
480 Lakatos et al., 2016; Michalareas et al., 2016). A recent study in rats demonstrated that low-
481 frequency LFP power (10-30 Hz) is negatively correlated with firing rate (Watson et al., 2018).
482 Therefore, it is possible that the β -oscillations exert an inhibitory function, similar to α -oscillations
483 (Spitzer and Haegens, 2017). Taken together, these studies suggest that α - and β -power may
484 reflect a similar function in regulating cortical excitability and perceptual decision-making.

485 In addition to detection accuracy, interval order (i.e. whether or not stimulus is presented in
486 the first interval) was also related to low-frequency power (Figure 4a–c). In the detection task,

487 low-frequency pre-stimulus power averaged across first and second intervals (P_{ave}) was signifi-
488 cantly greater in trials when a stimulus was presented in the first interval (T1 trials) relative
489 to trials when it was presented in the second interval (nT1 trials; Figure 4a). During T1 trials,
490 low-frequency synchronization (Kalcher and Pfurtscheller, 1995) induced by the stimulus in the
491 first interval probably leaked into the pre-stimulus period of the second, stimulus-absent interval.
492 Conversely, during nT1 trials, low-frequency desynchronization due to temporal expectation and
493 attention (Rohenkohl and Nobre, 2011) following the first, stimulus-absent interval leaked into
494 the pre-stimulus period of the second, stimulus-present interval. Including the interval order in
495 our regression model ensured that the effect of accuracy on oscillatory power was independent of
496 effects of interval order.

497 **Within-trial fluctuations of excitability**

498 Past studies on the relationship between perception and excitability have typically analyzed how
499 differences in perceptual reports were related to differences in pre-stimulus power *across* trials
500 (e.g. Busch et al., 2009; Iemi et al., 2017; Limbach and Corballis, 2016). This across-trial ap-
501 proach treats individual trials as independent samples and therefore ignores the fact that data are
502 collected in temporal order. This is potentially problematic, because it is known that both per-
503 ceptual reports and excitability change over the course of an experiment. Specifically, behavioral
504 measures such as hit rate (Boncompagni et al., 2016; Carrasco-López et al., 2017) and sensitivity
505 (Maniscalco et al., 2017) tend to decrease over time, possibly due to progressive fatigue, resulting
506 from an exhaustion of cognitive resources. Likewise, ongoing α -power tends to increase over the
507 course of an experiment (van Dijk et al., 2008), suggesting a decrease in excitability, possibly
508 as a result of fatigue (Kaida et al., 2006). Since perceptual reports and excitability both covary
509 across time, e.g. as a function of fatigue, their correlation could be epiphenomenal. Therefore,
510 several studies have tried to rule out that the across-trial correlation between performance and
511 α -power is confounded by fatigue by showing that the temporal factor does not explain the effect
512 on performance (van Dijk et al., 2008; Mathewson et al., 2009).

513 To test the bias models in our study, we used a different approach and quantified the differences
514 in excitability between two intervals *within* a trial (P_{rel}), instead of the differences in the absolute
515 magnitude of excitability *across* trials. This approach ensures that our measure of excitability is
516 not influenced by fatigue-related effects occurring over longer time scales. Crucially, our results

517 show a significant correlation between excitability and perceptual reports, even when the effects
518 of fatigue are ruled out. This study thus confirms that the relationship between excitability and
519 perception is not determined by fatigue.

520 **Perceptual bias and selective stimulus processing**

521 It is important to note that the present study focused on spontaneous, moment-to-moment
522 fluctuations in oscillatory power and, in turn, of neuronal excitability and inhibition. To this end,
523 the task was designed such that participants could not expect and selectively attend to a specific
524 time interval, spatial location, or stimulus feature. Therefore, our finding that spontaneous,
525 non-selective fluctuations in oscillatory power are associated with a perceptual bias rather than
526 a change in precision or accuracy, does not exclude the possibility that this bias *can* serve to
527 improve accuracy when the task allows for some form of selective stimulus processing.

528 Numerous studies have demonstrated that selective attention to a spatial location or to other
529 stimulus aspects allows for a selective gating of the task-relevant information by adjusting α -
530 power in task-relevant vs. irrelevant neuronal populations (see Foxe and Snyder, 2011, for a
531 review). When subjects are instructed to selectively attend to a spatial location, α -power de-
532 creases in the contralateral relative to the ipsilateral hemisphere, indicating greater excitability in
533 the task-relevant hemisphere and greater inhibition in the task-irrelevant hemisphere (Thut et al.,
534 2006; Busch and VanRullen, 2010). For example, Händel et al. (2011) demonstrated that this
535 lateralization serves to inhibit distracting stimuli in the unattended visual hemifield. Moreover,
536 selective attention to a particular stimulus feature (orientation vs. identity; Jokisch and Jensen,
537 2007), modality (visual vs. auditory; Mazaheri et al., 2014), and timing (expected vs. unex-
538 pected; Rohenkohl and Nobre, 2011) induces a relative increase of α -power in the currently
539 task-irrelevant areas.

540 Thus, our finding is consistent with the gating-by-inhibition account by Jensen and Mazaheri
541 (2010) and the pulsed-inhibition account by Mathewson et al. (2011). Both models argue that the
542 inhibitory effect of α -oscillations is not sustained, but pulsed as a function of α -phase, and that the
543 inhibitory phase is more pronounced than the excitatory counterpart. Moreover, both models argue
544 that top-down control can modulate both power and phase for selective information processing.
545 In light of the present findings, we propose that the performance-modulating effect of top-down

546 controlled α -oscillations is associated with a selective perceptual bias, which dampens responses
547 in those neuronal populations processing potentially distracting or task-irrelevant information.

548 **Conclusions**

549 We propose that the current state of neuronal excitability—indexed by spontaneous α - and β -
550 oscillations—biases the observer's subjective perceptual experience, by amplifying or attenuating
551 sensory representations, rather than the decision strategy.

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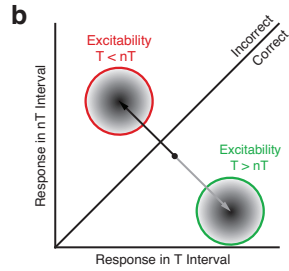
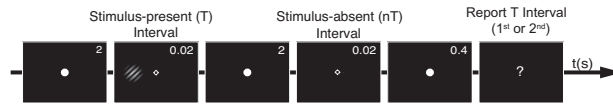
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a 2IFC Detection



c 2IFC Discrimination

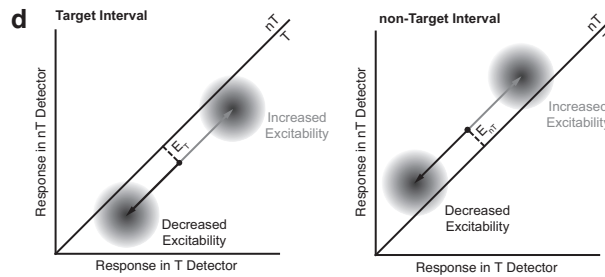
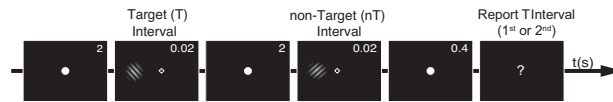


Figure 1: Effects of perceptual bias on 2IFC detection and discrimination performance according to signal detection theory (SDT). See Methods for predictions of the precision and decision bias model. **a:** in 2IFC detection, a target stimulus (T) appears in either one of two successive intervals and the task is to report which interval contained the stimulus. **b:** according to SDT, the internal response in the stimulus-present interval, R_T , is compared to the internal response in the non-target, stimulus-absent interval, R_{nT} , and the interval yielding the stronger response is reported. If $R_T > R_{nT}$ (below diagonal), the report is correct, otherwise incorrect. The perceptual bias model predicts that the accuracy of 2IFC detection reports is affected by the balance of excitability and inhibition between the stimulus-present and stimulus-absent intervals: weaker oscillatory power (i.e. stronger excitability) before the stimulus-present interval relative to before the stimulus-absent interval, is expected to boost detection accuracy (green circle); instead, stronger oscillatory power (i.e. stronger inhibition) before the stimulus-present interval relative to before the stimulus-absent interval, is expected to impair accuracy (red circle). **c:** in 2IFC discrimination, two successive intervals contain either a target (T) or a non-target (nT) stimulus and the task is to report in which interval the target was presented. **d:** according to SDT, for each interval, the difference between the internal responses of the target detector and non-target detector (i.e. distance from the diagonal; dashed line) represents the evidence of target presence in that interval (E), and the interval yielding stronger target-evidence is reported. If there is more target-evidence in the target interval, the response is correct, otherwise incorrect. The perceptual bias model predicts that increased excitability or inhibition in the target interval (left panel) or non-target interval (right panel) affects both target and non-target detectors equally, leaving target evidence in that interval unchanged (illustrated by shift parallel to the diagonal without affecting the distance to the diagonal). Thus, this model predicts that between-interval fluctuations of excitability do not affect 2IFC discrimination accuracy.

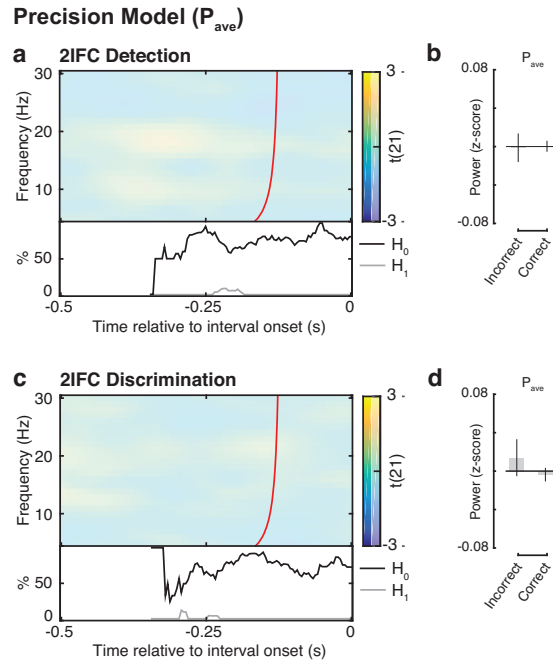


Figure 2: Relationship between overall oscillatory power (P_{ave}) and 2IFC accuracy; test of the precision model. **a/c:** Group-level t-statistics maps of the regression coefficient β_1 , indicating the relationship between accuracy and P_{ave} , in 2IFC detection and discrimination, respectively. Accuracy in neither 2IFC detection nor discrimination is related to P_{ave} . This null effect is corroborated by the BF analysis, indicating that there is more evidence supporting the H_0 than supporting the H_1 (bottom insets). The maps in **a/c** are averaged across the electrodes comprising the cluster of significant effects illustrated in figure 3a/c and masked by a p-value of 0.01 using two-sided cluster permutation testing. Time 0 s indicates interval onset. The red line in **a/c** indicates the time points before which oscillatory activity is not contaminated by activity after interval onset (lemi et al., 2017). **b/d:** Group-average P_{ave} in detection (**b**) and discrimination (**d**), shown separately for correct and incorrect trials, normalized by the P_{ave} in all trials. The bar plots are shown for illustrative purposes for the cluster of significant effects illustrated in figure 3a/c. These results refute the prediction of the precision model that low P_{ave} is related to higher accuracy.

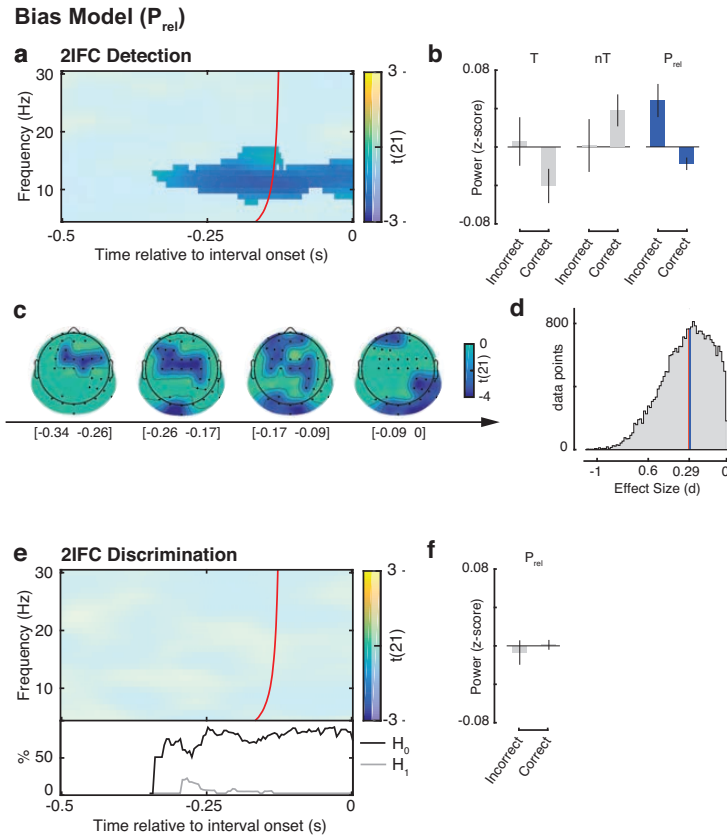


Figure 3: Relationship between relative oscillatory power (P_{rel}) and 2IFC accuracy; test of the perceptual bias and decision bias models. **a:** Group-level t-statistics maps of the regression coefficient β_1 , indicating the relationship between 2IFC detection accuracy and P_{rel} . Correct performance is related to lower 8–17 Hz P_{rel} , i.e. reduced α - and β -power preceding the stimulus-present interval relative to that preceding the stimulus-absent interval. **b:** Group-average power averaged across the window before the target interval (left panel) or that before the non-target interval (middle panel), shown separately for correct and incorrect 2IFC detections, normalized by the average power in all trials. Group-average P_{rel} (right panel) shown separately for correct and incorrect trials, normalized by the average P_{rel} in all trials. **c:** a time-course of topographies of the significant negative cluster. Black dots represent cluster electrodes. **d** Histogram of the effect size, estimated as Cohen's d, for the data within the time-frequency-electrode cluster of significant negative effects. The median value is highlighted by the blue vertical bar. **e:** Group-level t-statistics maps of the regression coefficient β_1 , indicating the relationship between 2IFC discrimination accuracy and P_{rel} . 2IFC discrimination accuracy is not related to P_{rel} . This null effect is corroborated by the BF analysis, indicating that there is more evidence supporting the H_0 than supporting the H_1 (bottom inset). **f:** Group-average P_{rel} shown separately for correct and incorrect 2IFC discriminations, normalized by the average P_{rel} in all trials. The maps in **a/e** are averaged across the electrodes comprising the cluster of significant effects illustrated in **a/c** and masked by a p-value of 0.01 using two-sided cluster permutation testing. Time 0 s indicates interval onset. The red line in **a/e** indicates the time points before which oscillatory activity is not contaminated by activity after interval onset (lemi et al., 2017). The plots in **b/f** are shown for illustrative purposes for the cluster of significant effects illustrated in **a/c**. The negative relationship between P_{rel} and accuracy in 2IFC detection, but not in 2IFC discrimination, confirms the perceptual bias model.

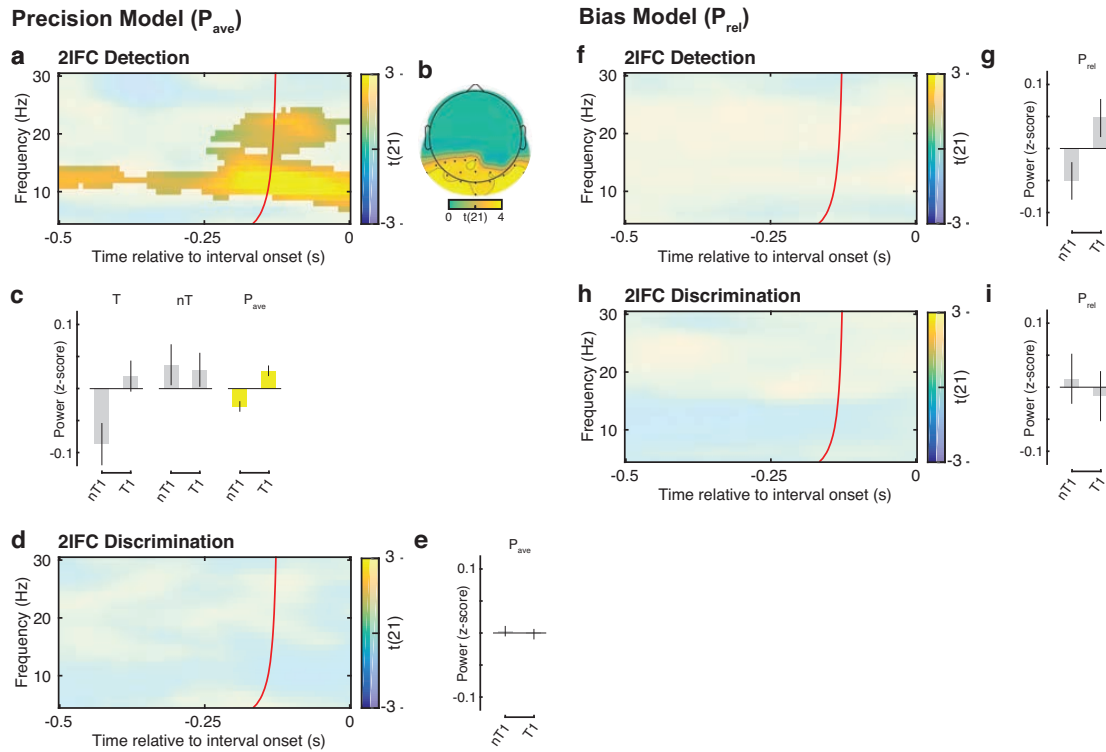
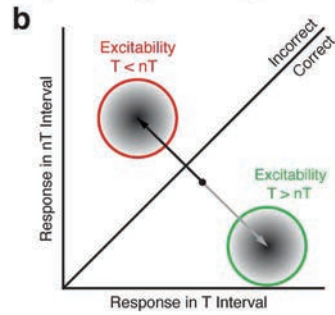
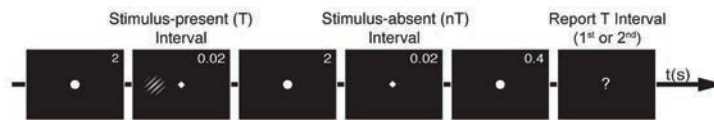
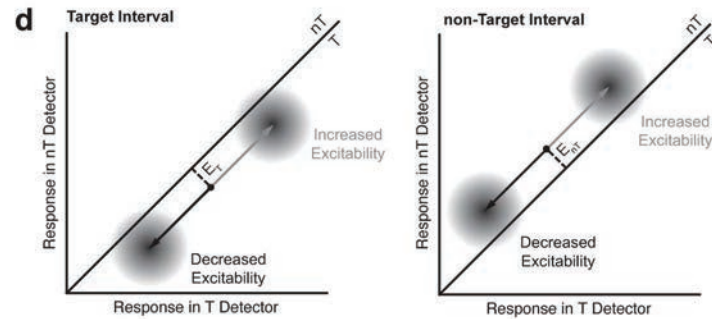
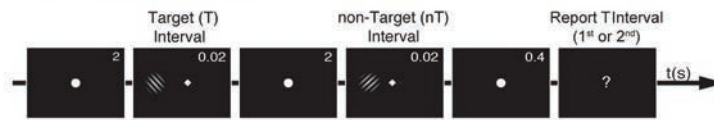


Figure 4: Relationship between oscillatory power (P_{ave} and P_{rel}) and interval order in 2IFC detection and discrimination. **a/d:** Group-level t-statistics map of the regression coefficient β_2 , indicating the relationship between interval order and P_{ave} in 2IFC detection and discrimination, respectively. **b:** Topography of the significant positive cluster in 2IFC detection. Black dots represent cluster electrodes. **c:** Group-average power averaged across the window before the stimulus-present interval (left panel) or that before the stimulus-absent interval (middle panel), shown separately for non-target first (nT1) and target first (T1) trials, normalized by the average power in all trials. Group-average P_{ave} (right panel) shown separately for nT1 and T1 detection trials, normalized by the average P_{ave} in all trials. **f/h:** Group-level t-statistics map of the regression coefficient β_2 , indicating the relationship between interval order and P_{rel} in 2IFC detection and discrimination, respectively. **g/i:** Group-average P_{rel} shown separately for nT1 and T1 trials, normalized by the average P_{rel} in all trials in 2IFC detection and discrimination, respectively. The maps in **a/d/f/h** are averaged across the electrodes comprising the cluster of significant effects illustrated in **a/b** and masked by a p-value of 0.01 using two-sided cluster permutation testing. Time 0 s indicates interval onset. The red line in **a/d/f/h** indicates the time points before which oscillatory activity is not contaminated by activity after interval onset (Lemi et al., 2017). The plots in **c/e/g/i** are shown for illustrative purposes for the cluster of significant effects illustrated in **a/b**. nT1: trials with non-target in the first interval; T1: trials with target in the first interval.

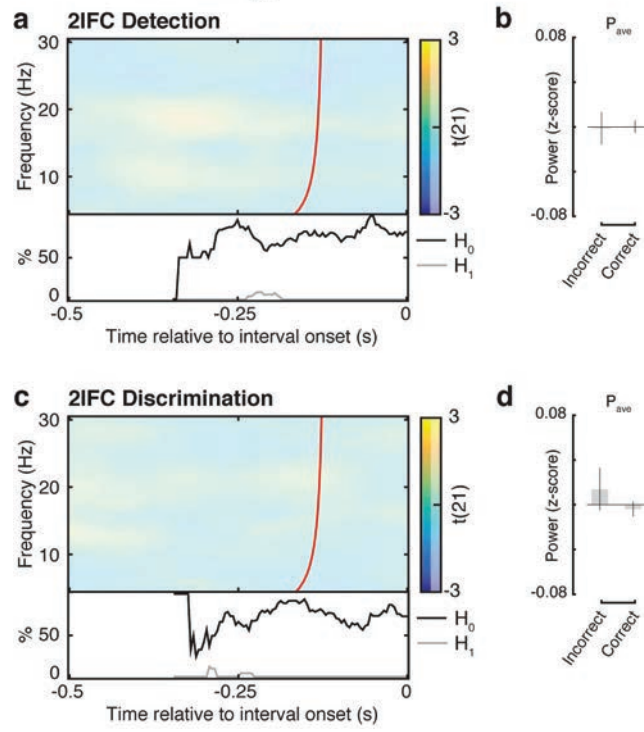
a 2IFC Detection

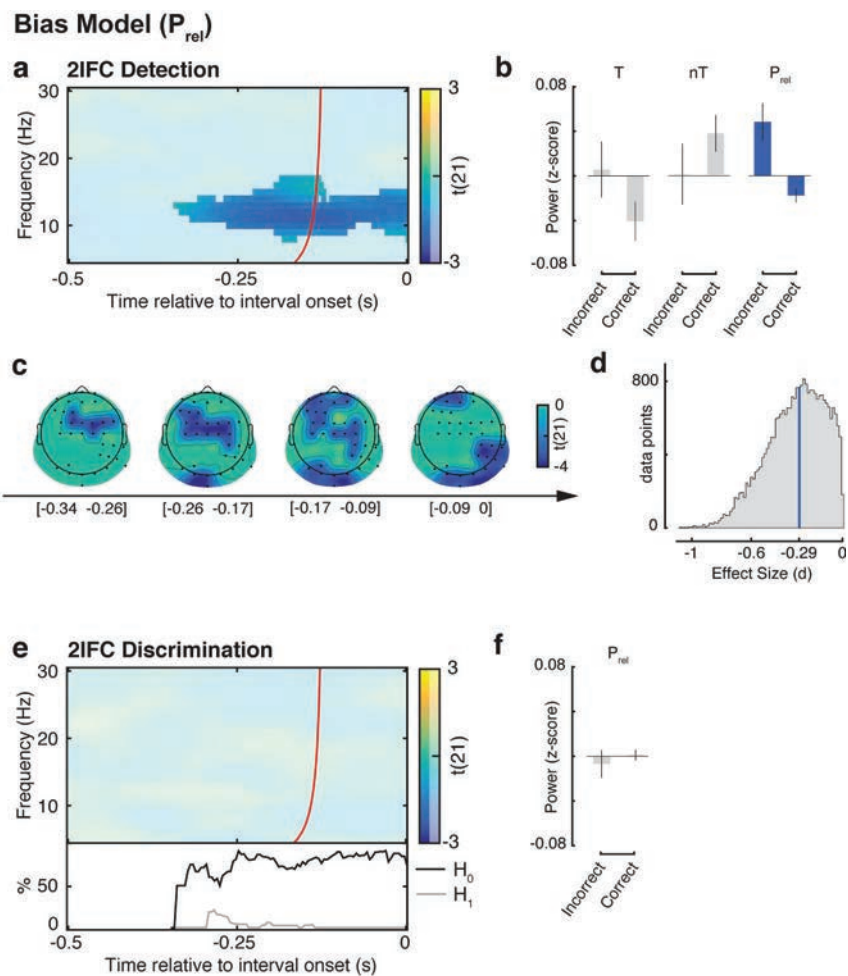


c 2IFC Discrimination

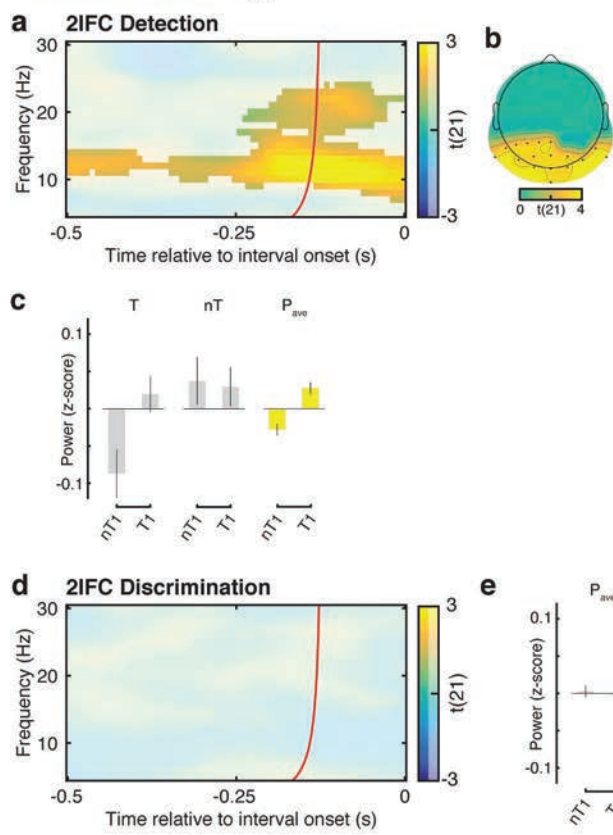


Precision Model (P_{ave})





Precision Model (P_{ave})



Bias Model (P_{rel})

