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Activity patterns in the neuropil of striatal cholinergic interneurons in freely moving mice represent their collective spiking dynamics

Rotem Rehani¹, Yara Atamna¹, Lior Tiroshi¹, Wei-Hua Chiu¹, José de Jesús Aceves Buendía¹, Gabriela J. Martins², Gilad A. Jacobson¹ and Joshua A. Goldberg¹

¹*Department of Medical Neurobiology, Institute of Medical Research Israel – Canada, The Faculty of Medicine, The Hebrew University of Jerusalem, 9112102, Jerusalem, Israel*

²*Zuckerman Mind Brain Behavior Institute, Columbia University, New York, NY, 10027, USA*

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Correspondence should be addressed to Joshua A. Goldberg, E-mail: joshg@ekmd.huji.ac.il.

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8 **Rotem Rehani^{1†}, Yara Atamna^{1†}, Lior Tiroshi^{1†}, Wei-Hua Chiu¹, José de Jesús**
9 **Aceves Buendía^{1‡}, Gabriela J. Martins², Gilad A. Jacobson¹ and Joshua A.**
10 **Goldberg¹**
- 11 ¹Department of Medical Neurobiology, Institute of Medical Research Israel – Canada, The
12 Faculty of Medicine, The Hebrew University of Jerusalem, 9112102, Jerusalem, Israel
13 ²Zuckerman Mind Brain Behavior Institute, Columbia University, New York, NY, 10027, USA
14 [†]Equal Contribution
15 [‡]Current Address: Departamento de Neurología y Psiquiatría, Instituto Nacional de Ciencias Médicas y
16 Nutrición Salvador Zubiran, INCMNSZ, Mexico
- 17 4. Author Contributions:
18 RR, YA, LT, GJM, GAJ and JAG designed research; RR, YA, LT, W-HC and JJAB performed
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37 **Abstract**

38 Cholinergic interneurons (CINs) are believed to form synchronous cell assemblies
39 that modulate the striatal microcircuitry and possibly orchestrate local dopamine release.
40 We expressed GCaMP6s, a genetically encoded calcium indicator (GECIs), selectively in
41 CINs, and used microendoscopes to visualize the putative CIN assemblies in the dorsal
42 striatum of freely moving mice. The GECI fluorescence signal from the dorsal striatum was
43 composed of signals from individual CIN somata that were engulfed by a widespread
44 fluorescent neuropil. Bouts of synchronous activation of the cholinergic neuropil revealed
45 patterns of activity that preceded the signal from individual somata. To investigate the
46 nature of the neuropil signal and why it precedes the somatic signal, we target-patched
47 GECI-expressing CINs in acute striatal slices in conjunction with multiphoton imaging or
48 wide-field imaging that emulates the microendoscopes' specifications. The ability to detect
49 fluorescent transients associated with individual action potential was constrained by the
50 long decay constant of GECIs (relative to common inorganic dyes) to slowly firing (< 2
51 spikes/s) CINs. The microendoscopes' resolving power and sampling rate further
52 diminished this ability. Additionally, we found that only back-propagating action potentials
53 but not synchronous optogenetic activation of thalamic inputs elicited observable calcium
54 transients in CIN dendrites. Our data suggest that only bursts of CIN activity (but not their
55 tonic firing) are visible using endoscopic imaging, and that the neuropil patterns are a
56 physiological measure of the collective recurrent CIN network spiking activity.

57

58 **Significance Statement**

59 Cholinergic interneurons (CINs) are key modulators of the striatal microcircuitry
60 that are necessary for assigning action value and behavioral flexibility. We present a first
61 endoscopic imaging study of multiple molecularly identified CINs in freely moving mice.
62 We reveal the presence of activity patterns in the CIN neuropil. We then use *ex vivo*
63 electrophysiological and imaging techniques to show that the neuropil signal is the
64 integrated fluorescence arising from the axo-dendritic arbors of CINs dispersed throughout
65 the striatum. We conclude that the neuropil signal acts as a mean-field readout of the
66 striatal CIN network activity.

67

68 **Key Words:**

69 local field potential (LFP); spatiotemporal patterns; gradient refractive index (GRIN) lens;
70 two-photon laser scanning microscopy; pacemaker; channelrhodopsin-2

71

72 **Introduction**

73 Striatal cholinergic interneurons (CINs) are the main population of tonically active
74 neurons (TANs) whose pause response is associated with the presentation of reward or
75 with stimuli that are associated with reward (Anderson, 1978; Kimura et al., 1984; Aosaki
76 et al., 1994; Raz et al., 1996). It was hypothesized long ago that CINs form synchronous
77 striatal cell assemblies during the pause responses (Graybiel et al., 1994). These assemblies
78 collectively modulate neuronal excitability, synaptic transmission and synaptic plasticity in
79 the striatal microcircuitry (Calabresi et al., 2000; Pakhotin and Bracci, 2007; Pisani et al.,
80 2007; Goldberg et al., 2012; Plotkin and Goldberg, 2018). This hypothesis has been

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81 buttressed by recent *ex vivo* data showing that synchronous activation of CINs can lead to
82 the release of dopamine, GABA and glutamate in the striatum (Cachope et al., 2012; English
83 et al., 2012; Threlfell et al., 2012; Chuhma et al., 2014; Nelson et al., 2014). Multiple
84 electrode recordings in primates have shown that TANs exhibit some degree of synchrony
85 which increases in experimental parkinsonism (Raz et al., 1996; Apicella et al., 1997;
86 Goldberg et al., 2002; Ravel et al., 2003; Goldberg et al., 2004). With the advent of
87 genetically encoded calcium indicators (GECIs) it is now possible to conduct longitudinal
88 studies on large assemblies of molecularly identified neurons, such as the CINs, in freely
89 moving mice performing self-initiated movements or undergoing training (Mank and
90 Griesbeck, 2008; Ghosh et al., 2011; Lin and Schnitzer, 2016). In most GECI experiments,
91 the images are composed of fluorescence that arises from the somata of the targeted
92 neurons and due to background fluorescence.

93 In most studies the background activity is presumed to arise from out-of-focus
94 neurons, hemodynamics (due to the auto-fluorescence of blood vessels) and other artifacts
95 such as motion or photo-bleaching of dyes (Pnevmatikakis et al., 2016; Zhou et al., 2018). In
96 the case of microendoscopic imaging with GRIN lenses implanted deep in the brain and
97 where diffuse light contamination can be minimized, the contribution of hemodynamics is
98 likely to be less of an issue (Ma et al., 2016). Nevertheless, most recent studies from various
99 groups that conduct microendoscopic imaging have adopted a strategy that calls for the
100 removal of the background signal in order to extract a cleaner neuronal signal. Two
101 approaches have been used to subtract the background signal. The first is a heuristic and
102 involves estimating the background fluctuations in the vicinity of a given soma. This signal
103 (or a weighted version of it) is subtracted from the somatic signal (Klaus and Plenz, 2016;

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104 Stamatakis et al., 2018; Zhou et al., 2018). The logic is simple. Due to the substantial depth-
105 of-field of the imaging system, any signal observed in the vicinity is likely to contaminate
106 the pixels in the soma and must therefore be subtracted. The other approach builds on the
107 fact that the background signal tends to be highly correlated in space, and therefore lends
108 itself to being modeled as a global background signal composed of a DC term plus some low
109 spatial frequency components. By adding this assumption to an assumption regarding the
110 parametric exponential shape of calcium events that accompany individual spikes, this
111 approach has yielded sophisticated algorithms which simultaneously estimate independent
112 neuronal sources while subtracting a global model of the background (Klaus and Plenz,
113 2016; Stamatakis et al., 2018; Zhou et al., 2018).

114 However, when transfecting the neurons, the fluorescent proteins are expressed in
115 all compartments of the neurons including the axon and dendrite (Kerr et al., 2005; Lee et
116 al., 2017). When considering the known anatomy of CINs that possess very intricate axonal
117 and dendritic arbors (Chang et al., 1982; DiFiglia, 1987; Wilson et al., 1990; Kawaguchi,
118 1992), it stands to reason that a large component of the background signals is not out-of-
119 focus somatic signals but rather calcium influx due to propagation and/or back-
120 propagation action potentials throughout the CINs' axonal and dendritic arbors,
121 respectively. Under these circumstances, these background signals should be tightly related
122 to the network state of the CIN network, implying that the background signal could provide
123 a physiological readout of the entire CIN network.

124 In the current study, we describe GECI signals from striatal cholinergic neuropil in
125 freely moving mice imaged with microendoscopes. In order to better understand the origin
126 of the neuropil signal we use wide field ("one-photon") and two-photon laser scanning

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127 microscopy (2PLSM) imaging of GECI signals from CINs in acute striatal slices. The
128 combination of approaches leads us to the conclusion that to a large degree the patterns
129 observed in the cholinergic neuropil arise from back-propagating APs (bAPs) in the
130 dendritic arbors. As a sum of many cholinergic processes the background activity, like local
131 field potentials (LFPs), represents a readout of the collective discharge of CINs.

132

133 **Materials and Methods**

134 **Animals**

135 Experimental procedures adhered to and received prior written approval from the
136 The Hebrew University's Institutional Animal Care and Use Committee. Two-to-nine-
137 months-old choline acetyltransferase-cre dependent (ChAT-IRES-Cre) transgenic mice
138 (stock number 006410; Jackson Laboratories, Bar Harbor, ME, USA) of both sexes were
139 used in the experiments.

140 **Stereotaxic injection of adeno-associated viruses and ChR2**

141 Mice were deeply anesthetized with isoflurane in a non-rebreathing system (2.5%
142 induction, 1–1.5% maintenance) and placed in a stereotaxic frame (model 940, Kopf
143 Instruments, Tujunga, CA, USA). Temperature was maintained at 35°C with a heating pad,
144 artificial tears were applied to prevent corneal drying, and animals were hydrated with a
145 bolus of injectable saline (5 ml/kg) mixed with an analgesic (5 mg/kg carprofen). To
146 calibrate specific injection coordinates, the distance between bregma and lambda bones
147 was measured and stereotaxic placement of the mice was readjusted to achieve maximum
148 accuracy. A small hole was bored into the skull with a micro drill bit and a glass pipette was
149 slowly inserted at the relevant coordinates in aseptic conditions. To minimize backflow,

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150 solution was slowly injected and the pipette was left in place for 7 min before slowly
151 retracting it.

152 A total amount of 400 nl of an adeno-associated virus serotype 9 harboring
153 GCaMP6s construct (AAV9-syn-flex-GCaMP6s; $> 2.5 \times 10^{13}$ viral genome/ml; University of
154 Pennsylvania Vector Core, catalog number AV-9-PV2824) was injected into the dorsal
155 striatum under aseptic conditions. The coordinates of the injection were as follows:
156 anteroposterior, +0.5 mm; mediolateral, +2.3 mm; and dorsoventral, -2.8 mm, relative to
157 bregma using a flat skull position (Paxinos and Franklin, 2012).

158 For thalamic expression of ChR2 a total of 250 nl of an adeno-associated virus
159 serotype 9 harboring ChR2 construct (AAV9-hSyn-ChR2-eGFP; $> 2.5 \times 10^{13}$ viral
160 genome/ml; University of Pennsylvania Vector Core, catalog number AV-9-26973P) was
161 injected into the caudal intralaminar nucleus (ILN) of the thalamus to transfect the
162 parafascicular nucleus (PfN) neurons under aseptic conditions. The coordinates of the
163 injection were as follows: anteroposterior, -2.3 mm; mediolateral, +0.65 mm; and
164 dorsoventral, -3.35 mm, relative to bregma using a flat skull position (Paxinos and
165 Franklin, 2012; Ellender et al., 2013). Two to three weeks after viral injection mice were
166 used for experiments.

167 Gradient refractive index (GRIN) lens implantation

168 One week after the stereotaxic injection, mice were deeply anesthetized with
169 isoflurane in a non-rebreathing system and placed in the stereotaxic frame, as described
170 above (in some cases, a bolus of ketamine (32 mg/kg)-xylazine (3.2 mg/kg) was injected
171 initially to stabilize the preparation for and induction of anesthesia). A hole slightly wider
172 than the 1mm diameter (4 mm long) GRIN lens was drilled into the skull in aseptic

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173 conditions. We aspirated cortex with a 27-30 G needle to a depth of approximately 2 mm
174 (just past the corpus callosum) and then fit the lens in snugly and (dental-) cemented it into
175 place together with a head bar for restraining the mouse when necessary. One week later
176 we attached a baseplate to guarantee that the endoscope will be properly aligned with the
177 implanted GRIN lens. To ensure light impermeability, the dental cement was mixed with
178 coal powder and painted with black nail polish. Two weeks later, the freely-moving mice
179 were imaged in a behavior chamber lit by diffuse infrared light.

180 Microendoscopic Imaging

181 Microendoscopes (*nVista*, Inscopix, Palo Alto, CA, USA) sampled an area of
182 approximately 600 μm by 900 μm (pixel dimension: 1.2 μm) at 10 frames/sec. Movies were
183 motion corrected with the Inscopix Data Processing Software (IDPS) suite. Motion-
184 corrected movies and electrophysiological data were analyzed, and curve fitting was
185 performed using custom-made code in MATLAB (MathWorks, Natick, MA, USA). We
186 extracted fluorescence changes over time ($\Delta F/F$) such that $\Delta F/F \stackrel{\text{def}}{=} \frac{F-F_0}{F_0}$. F is the raw
187 fluorescent values recorded; F_0 denotes the minimal averaged fluorescence in 1.5 sec-
188 overlapping 3 sec periods throughout the measurement. Mice with weak transfection or
189 too few somata were discarded. Somata were identified from a long-term temporal
190 maximum projection of the $\Delta F/F$ signal, and Regions-of-Interest (ROIs) were marked
191 manually to engulf the somatic area. The annulus of each ROI was defined as a ring of pixels
192 with the same area as the ROI, whose inner diameter is the distance of the point on the
193 border of the ROI that is farthest away from the center-of-mass of the ROI plus 5 additional
194 pixels. These annuli were also used to estimate the collective neuropil signal. We used an
195 alternative scheme to estimate the collective signal. We considered all parts of the image that

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196 were devoid of somata and their surrounding 40 pixels. We then chose 100 circular ROIs with a
197 radius of 5 pixels randomly located within this region.

198 To determine the temporal relationship between the somatic and annular signals,
199 we detected major events in the somatic signal and averaged both the somatic and annular
200 signals around these times. Signals were first averaged over all of the events in each soma-
201 annulus pair, and the resulting traces were then averaged over the pairs. Our criterion for
202 choosing the pairs was that they must display at least 5 events that did not contain another event,
203 either in the soma or the annulus, within the 3 seconds following the peak.

204 Slice preparation

205 Two to three weeks following AAV injections, mice were deeply anesthetized with
206 intraperitoneal injections of ketamine (200 mg/kg) – xylazine (23.32 mg/kg) and perfused
207 transcardially with ice-cold modified artificial CSF (ACSF) oxygenated with 95% O₂-5%
208 CO₂ and containing the following (in mM): 2.5 KCl, 26 NaHCO₃, 1.25 Na₂HPO₄, 0.5 CaCl₂, 10
209 MgSO₄, 10 glucose, 0.4 Ascorbic acid, and 210 sucrose. The brain was removed and blocked
210 in the sagittal plane and sectioned at a thickness of 240 μm in ice-cold modified ACSF. Slices
211 were then submerged in ACSF, bubbled with 95% O₂-5% CO₂, and containing the following
212 (in mM): 2.5 KCl, 126 NaCl, 26 NaHCO₃, 1.25 Na₂HPO₄, 2 CaCl₂, 2 MgSO₄, and 10 glucose
213 and stored at room temperature for at least 1 h before recording and/or imaging.

214 Slice visualization and data collection – wide-field imaging

215 Slices were transferred to a recording chamber mounted on an Olympus BX51
216 upright, fixed-stage microscope and perfused with oxygenated ACSF at room temperature.
217 A 20X, 0.5 NA water immersion objective was used to examine the slice using Dodt contrast
218 video microscopy.

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219 **Electrophysiology:** Electrophysiological recordings were obtained with a Multiclamp 700B
220 amplifier (Molecular Devices, Sunnyvale, CA). The junction potential, which was 7–8 mV,
221 was not corrected. Signals were digitized at 10 kHz. Patch pipette resistance was typically
222 3–4 M Ω when filled with the recording solution. For calcium imaging experiments in
223 conjunction with current-clamp recordings the pipette contained the following (in mM):
224 130 K-gluconate, 6 KCl, 8 NaCl, 10 HEPES, 2Mg_{1.5}ATP, pH 7.3 with KOH (280–290
225 mOsm/kg).

226 **One-photon wide-field calcium imaging:** Optical measurements were made using 470 nm
227 LED illumination (Mightex, Toronto, ON, Canada) and a cooled EM-CCD (Evolve 512 Delta,
228 Photometrics, Tucson, AZ, USA). Frames were 512×512 pixels, pixel size was 0.4 μ m with
229 no binning and frame rate was 5-10 Hz. Regions of interest were marked manually offline
230 and fluorescent traces were extracted.

231 Optical and electrophysiological data were obtained using the custom-made
232 shareware package WinFluor (John Dempster, Strathclyde University, Glasgow, Scotland,
233 UK), which automates and synchronizes the imaging signals and electrophysiological
234 protocols. $\Delta F/F$ (for all acute slice experiments) was calculated as defined above with F_0
235 defined as the minimal value attained during the trace.

236 Slice visualization and data collection - 2PLSM

237 The slices were transferred to the recording chamber of Femto2D-Galvo scanner
238 multiphoton system (Femtonics Ltd., Budapest, Hungary) and perfused with oxygenated
239 ACSF at room temperature. A 16X, 0.8 NA water immersion objective was used to examine
240 the slice using oblique illumination.

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241 **Electrophysiology:** Electrophysiological recordings were obtained with a Multiclamp 700B
242 amplifier (Molecular Devices, Sunnyvale, CA). The junction potential, which was 7–8 mV,
243 was not corrected. Signals were digitized at 40 kHz. Patch pipette resistance and solution
244 were as described for one-photon experiments.

245 **2PLSM calcium imaging:** The 2PLSM excitation source was a Chameleon Vision 2 tunable
246 pulsed laser system (680–1,080 nm; Coherent Laser Group, Santa Clara, CA). Optical
247 imaging of GCaMP6s signals was performed by using a 920-nm excitation beam. The
248 GCaMP6s emission was detected and collected with gated GaAsP photomultiplier tubes
249 (PMTs) for high sensitivity detection of fluorescence photons as part of the Femto2D-Galvo
250 scanner. The laser light transmitted through the sample was collected by the condenser
251 lens and sent to another PMT to provide a bright-field transmission image in registration
252 with the fluorescent images. Line scans were marked through the somata and visible
253 dendrites and 20–250 Hz scans were performed, using $\sim 0.2\text{-}\mu\text{m}$ pixels and an 8–12 μs
254 dwell time. ROIs were marked manually offline based on the online marked line scans and
255 fluorescent traces were extracted.

256 Optical and electrophysiological data were obtained using the software package
257 MES (Femtonics), which also integrates the control of all hardware units in the microscope.
258 The software automates and synchronizes the imaging signals and electrophysiological
259 protocols. Data was extracted from the MES package to personal computers using custom-
260 made code in MATLAB.

261 Somatic current injection

262 To generate subthreshold depolarizations, we injected 8–12 pA for 800 ms such that
263 the voltage almost reached the threshold of activation. A 5 ms long, 500 pA pulse was used

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264 to generate an action potential. To calculate the calcium response to the stimulations we
 265 subtracted the baseline fluorescent level 50 ms prior to the stimulations and calculated the
 266 integrated $\Delta F/F$ over a duration 800 ms from the start time of the stimulation both for sub-
 267 and supra-threshold depolarizations.

268 **Spike triggered averaging (STA) and model**

269 To generate the STA, we averaged the $\Delta F/F$ signal around spike times. To fit the
 270 dependence of the amplitude of the STA on firing rate (Figure 5F) we used a
 271 phenomenological model. Let τ be the decay time constant of GCaMP. Assume a periodic
 272 neuron with an inter spike interval of duration T , such that $f=1/T$ is the firing frequency.
 273 The decay of the GCaMP fluorescence can be modeled as $e^{-\frac{1}{T\tau}}$. If F_0 is the baseline
 274 fluorescence level and ΔF is the amplitude of the fluorescence calcium trace visible over the
 275 baseline fluorescence, then the equation describing the decay of the GCaMP from its
 276 maximum value to baseline value is as follows:

$$(F_0 + \Delta F) \cdot e^{-\frac{1}{T\tau}} = F_0$$

$$\Leftrightarrow \frac{\Delta F}{F_0} = e^{\frac{1}{T\tau}} - 1$$

277

278 **Optogenetic stimulation**

279 Blue light LED of the Femto2D-Galvo scanner multiphoton system (473 nm,
 280 Femtonics) was used for full-field illumination. Light pulse trains consisted of 5 pulses at
 281 10 Hz, each pulse lasting 1ms. Fast gated GaAsP PMTs were used to prevent saturation of
 282 the PMTs due to the LED light flashes. The PMTs were disabled 5 ms prior to LED flash and
 283 re-enabled 5 ms after the end of the light flash. To calculate the calcium response in

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284 response to the optogenetic stimulation, we subtracted the baseline fluorescence prior to
285 the stimulations (50 ms prior to stimulation time), and compared the integrated dendritic
286 calcium signal during a 200 ms window beginning 500 ms after evoking sub-threshold
287 EPSPs, to the dendritic calcium signal generated by spontaneously occurring bAPs during
288 that same time window in the same neurons.

289 Immunohistochemistry

290 Mice were deeply anesthetized and perfused transcardially with 0.1 M phosphate
291 buffer (PB) followed by ice-cold 4% paraformaldehyde (PFA). Coronal sections of the
292 striatum were cut at 30 μm on a cryostat microtome (Leica CM1950) in antifreeze buffer
293 (1:1:3 volume ratio of ethyl glycerol, glycerol, and 0.1 M PB) and stored at -20°C before
294 further analysis. The sections were preincubated in 5% normal horse serum and 0.3%
295 Triton X-100 in 0.1 M PB for 40 min after washing steps, and incubated overnight at 4°C
296 with the primary antibodies [goat anti-choline acetyltransferase (ChAT), 1:100 (Millipore;
297 RRID: AB_262156)]. On the second day, sections were incubated with fluorophore-
298 conjugated species-specific secondary antibodies [donkey anti-goat, 1:1000 (Abcam)] for 2
299 h at room temperature. Brain sections were rinsed in PBS and directly cover-slipped by
300 fluorescent mounting medium (Vectashield, Vector Laboratories). Multilabeling fluorescent
301 immunostainings of juxtacellularly filled neurons were analyzed using a laser-scanning
302 microscope (LSM 510 Meta, Zeiss) using 20X/0.3 NA interference contrast lens (20X zoom).

303 Data and statistical analysis

304 Peak events in the spatial average were detected with a peak-finding algorithm (MATLAB)
305 with the condition that the peak amplitude be larger than 35% $\Delta F/F$.

306 The nonparametric two-tailed Wilcoxon signed-rank test (SRT) was used for
307 matched samples. Null hypotheses were rejected if the *P*-value was below 0.05.

308

309 **Results**

310 **Synchronous patterns in striatal cholinergic neuropil of freely moving mice**

311 The dorsolateral striatum (DLS) of choline acetyltransferase (ChAT)-cre mice was
312 transfected with adeno-associated viruses (AAVs) harboring cre-dependent CGaMP6s,
313 causing this genetically encoded calcium indicator (GECI) to express selectively in CINs
314 (Figure 1A). Following implantation of GRIN lens in the transfected area (Figure 1B),
315 imaging an area of approximately 600 μm by 900 μm through the lens using a miniaturized
316 endoscope in two freely-moving mice (Figure 1C) revealed spatiotemporal fluctuations in
317 fluorescence in the cholinergic neuropil. These fluctuations were characterized by
318 recurring, rapid bursts of activation that permeated the entire field-of-view (FoV) and that
319 slowly decayed (Movie 1). Embedded within the neuropil were several dozen somata of
320 individual CINs that also exhibited substantial fluctuations in fluorescence (Figure 1D). Due
321 to the depth-of-field of the 0.5 numerical aperture (NA) GRIN lens, the pixels from somata
322 also contain contributions of fluorescence from the dense, space-filling cholinergic
323 processes (Chang et al., 1982; DiFiglia, 1987; Wilson et al., 1990; Kawaguchi, 1992)
324 traversing above and below the somata and possibly from other out-of-focus fluorescent
325 somata. One expression of this is that the somatic fluctuations are always superimposed
326 upon the temporal fluctuations of the surrounding pixels that contain the same
327 contribution from the by-passing neuropil (Figure 1E, Movie 2).

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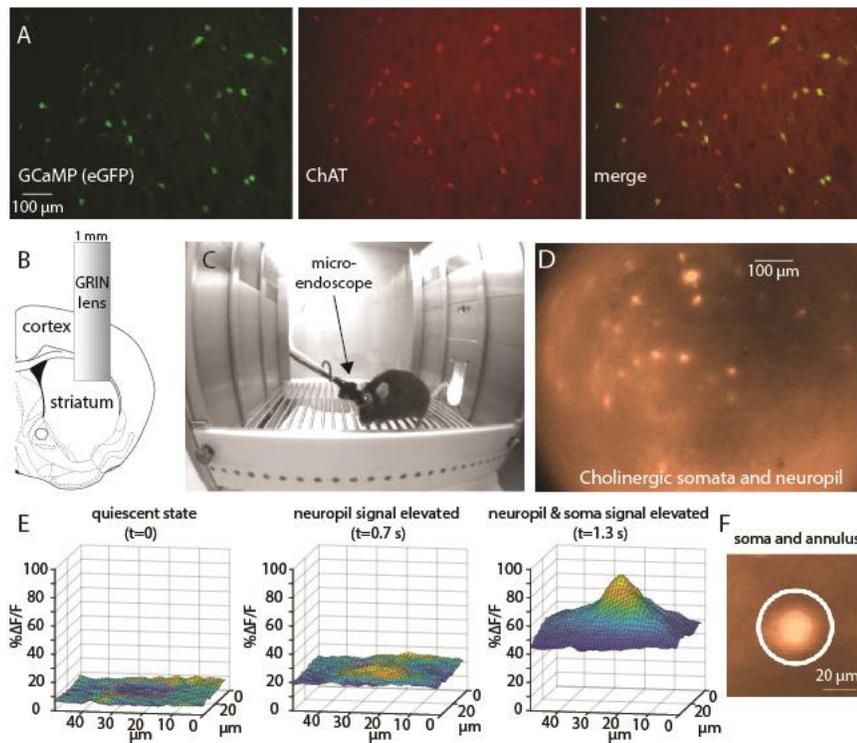


Figure 1. Imaging of the striatal cholinergic network in freely moving mice reveals both somatic and neuropil signals. A. Immunohistochemical analysis of dorsal striatum of choline acetyltransferase (ChAT)-cre mice stereotactically injected with adeno-associated viruses harboring floxed GCaMP6s demonstrates its selective expression in CINs. B. A 1 mm diameter GRIN lens is implanted into dorsolateral striatum following aspiration of cortical tissue. C. Implanted mouse with a microendoscope mounted on its head moves freely in a behavior chamber. D. Image via lens in freely moving mouse reveals a GCaMP6s signal from 44 identifiable somata and from the surrounding neuropil. E. 3-D rendition of a patch of the $\Delta F/F$ signal surrounding a soma reveals that an elevation in the neuropil signal precedes elevation of the somatic signal (region of soma indicated by a red circle). F. Illustration of the sampling of a somatic region-of-interest (central circle) and a surrounding (white) annular region.

328

329 To estimate the spatiotemporal structure of the neuropil signal and to compare it to
 330 the somatic activity, we analyzed activity in annuli surrounding each of the somata in the
 331 FoV (Figure 1F). In Figure 2A we depict a color-coded matrix of the fluctuations in
 332 fluorescence ($\Delta F/F$) as a function of time with each row representing an individual annulus.

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333 This matrix reveals that the neuropil signal is composed of dramatic increases in $\Delta F/F$ that
 334 are highly synchronous across the entire FoV (as is evident from the near-identical signal in
 335 the various rows of the matrix), and that decay slowly, as can be seen in the population
 336 average of all the annuli (Figure 2B, red trace). To justify the use of the annuli as a fair
 337 representation of the neuropil activity, we calculated the average signal that arises from
 338 100 small circular ROIs randomly located within the region of the image that is devoid of
 339 somata (See Materials and Methods). The resulting average (Figure 2B, gray trace) is
 340 indistinguishable for the average annuli signal. Thus, while the annuli signals reported the
 341 global neuropil signal, the individual somata exhibited more distinct dynamics, once the
 342 signal from each annulus was subtracted from its corresponding soma (Figure 2C).

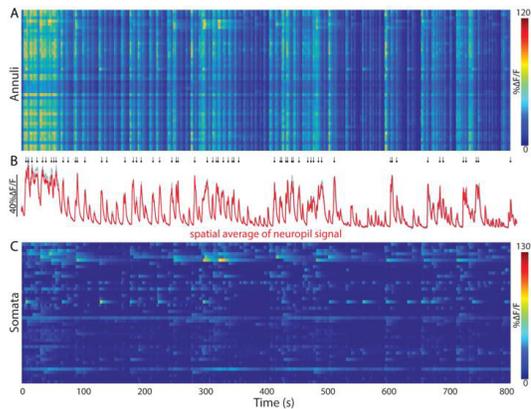


Figure 2. Cholinergic neuropil signal in dorsolateral striatum in freely moving mouse. A. Color coded matrix of activity of neuropil $\Delta F/F$ signal sampled from the annuli surrounding 44 somata scattered in the field-of-view. Time is represented along the horizontal axis. Each row corresponds to an individual annulus. B. population average of signals from all annuli (red, using annuli associated with the somata; gray – using randomly located circular ROIs that are far from any soma). Arrows above represent peaks of strong network activation (see Materials and Methods). C. Color coded activity of the 44 somata $\Delta F/F$ signals, after subtraction of the surrounding annular signal.

343

344

345

346 **The neuropil calcium signal precedes the somatic signal**

347 As seen above (Figure 1E, Movie 2), comparison of the activity of a given soma (after
348 subtraction) and its surrounding neuropil signal (taken from the corresponding annulus)
349 suggests that even though the activity of the ROI and annulus are quite distinct, every time
350 a soma is activated, this activation is preceded slightly by an activation of the surrounding
351 neuropil signal (Figure 3A). To quantify this effect, we calculated for 44 soma-annulus
352 pairs, the event-triggered average of the annulus signal around the time of an event in its
353 corresponding soma. The population average (across all 44 pairs) shows that each somatic
354 event is preceded on average by a rise in the neuropil signal that begins 2 seconds earlier
355 (Figure 3B). The neuropil also decays faster than the somatic signals (Figure 3C, median
356 somata: 4.35 sec, median annuli: 2.32 sec, $n=14$ eligible pairs, $P = 3.7 \times 10^{-4}$, SRT). Given
357 that the cholinergic neuropil is almost entirely intrinsic to the striatum (Mesulam et al.,
358 1992; Contant et al., 1996; Dautan et al., 2014), it is unclear why the neuropil signal would
359 begin prior to the somatic signals. Perhaps the neuropil signal precedes the somatic signals
360 because the former represents input to the latter. It is possible that activation of synaptic
361 inputs generates elevations in dendritic calcium levels that would manifest themselves as
362 neuropil signals that precede the somatic discharge. Alternatively, perhaps the afferent
363 cholinergic projection from the pedunculopontine nucleus to DLS (Dautan et al., 2014) was
364 infected retrogradely by the striatal AAV injection and contributes to the fluorescence,
365 thereby contributing to a fluorescent neuropil signal that precedes the somatic signal.
366 However, these possibilities seem unlikely because 2 seconds is too long a latency to be
367 accounted for simply by synaptic delays.

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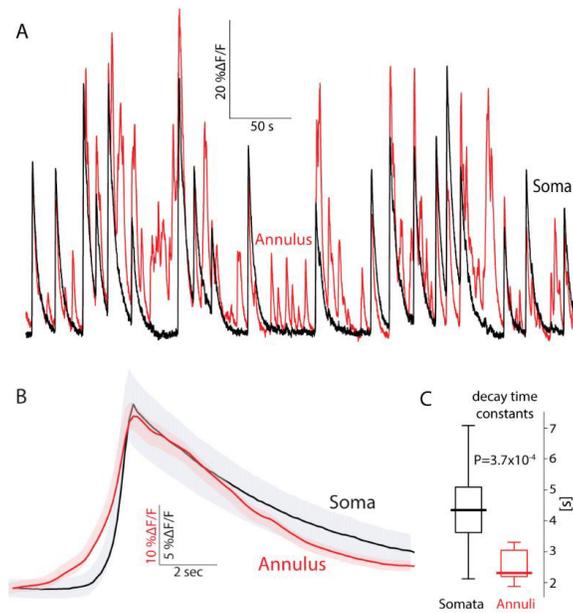


Figure 3. Annular (neuropil) signal precedes somatic signal in freely moving mice. A. Calcium ($\Delta F/F$) signal from a soma-annulus pair. B. Average calcium signal from the soma and its corresponding annulus averaged over soma-annulus pairs triggered on the somatic calcium events. Shaded areas mark the 95 percent confidence intervals. C. Boxplot of decay time constants of somatic vs. annular calcium signals. Bold line is the median and the whiskers are the 25th and 75th percentiles.

368 Several properties of the neuropil and somatic signals are therefore still in need of
 369 elucidation. How are fluctuations in somatic fluorescence signals related to the actual
 370 discharge of cholinergic interneurons? What is the physiological process that generates the
 371 neuropil signal? What is the origin of the 2 second long neuropil activity that precedes the
 372 somatic signals? These questions prompted us to delve deeper into the origin of the
 373 somatic and neuropil signals generated during the collective activity of CINs.

374 Because CINs are autonomously active neurons (Bennett and Wilson, 1999;
 375 Surmeier et al., 2005), we reasoned that some degree of collective cholinergic activity
 376 would be preserved in acute striatal slices, and that we could image this activity in the
 377 ChAT-cre mice expressing GCaMP6s selectively in CINs. We also reasoned that using two-
 378 photon laser scanning microscopy (2PLSM) would help us discriminate between somatic
 379 and neuropil signals. Due to the miniscule depth-of-field ($<2 \mu\text{m}$ FWHH) of 2PLSM, the

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380 contamination of somatic imaging by out-of-focus neuropil would be negligible.
381 Additionally, 2PLSM allows imaging of individual dendrites which are presumably a major
382 contributor to the neuropil signal, and study precisely under what circumstances they give
383 rise to GCaMP6s signals. By combining targeted patch clamp recordings with 2PLSM
384 imaging we could address mechanistic questions regarding the relationship of the
385 somatodendritic calcium signal and the electrophysiological activity of the CINs.

386 Somatic GCaMP6s signals exhibit diverse temporal patterns of activity *ex vivo*

387 2PLSM imaging of acute striatal slices demonstrated that neuropil expressing
388 fluorescent GCaMP6s could be observed. Moreover, the neuropil can be resolved as
389 dendritic (and perhaps axonal) processes. The striations were devoid of GCaMP6s, in line
390 with their known composition of non-cholinergic afferent fibers (Wilson, 2004). Embedded
391 within the fluorescent neuropil processes several (up to 10 per experiment) CIN somata
392 could be visualized. In the example depicted in Figure 4A, we were able to manually mark 9
393 distinct somata for imaging and extract traces of $\Delta F/F$ that exhibited autonomous calcium
394 fluctuations in the transfected neurons (Figure 4B). In some traces, calcium transients that
395 appear to correspond to individual action potentials could be observed (top 3 traces).
396 Collectively, these traces demonstrated that the temporal structure of the fluctuations
397 varied considerably among the somata (Figure 4B), with some cells exhibiting large
398 fluctuations in $\Delta F/F$ while others exhibited relatively uneventful traces (bottom 5 traces).
399 Interestingly, the nature of the calcium signal in individual neurons could vary
400 considerably with time. For example, one CIN (marked by the pink arrow in Figure 4C)
401 exhibited large calcium fluctuations in the initial trace (Figure 4D, upper pink trace). A few
402 minutes later, these fluctuations died down (middle pink trace). Finally, after a few more

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403 minutes elapsed, large fluctuations resumed (bottom pink trace). Such findings are
 404 consistent with previous studies that showed that individual CINs in acute slices can
 405 change their firing pattern from regular to irregular to bursting discharge (Bennett and
 406 Wilson, 1999).

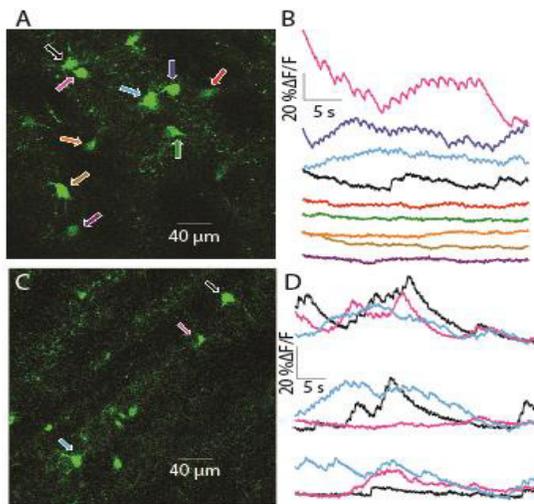


Figure 4. 2PLSM imaging of CIN somata in acute striatal slices. A. 2PLSM image of CINs expressing GCaMP6s in an acute striatal slice. Nine individual CINs are identified and color coded with arrows. B. Color coded traces of calcium ($\Delta F/F$) signals from the 9 cells depicted in panel A. C. 2PLSM image from another mouse, with three identified and color-coded CINs. D. Three repetitions of calcium imaging of the 3 CINs depicted in panel C – a few minutes apart.

407 It is easy to make a convincing case that the GCaMP6s signal represents autonomous
 408 discharge when transients associated with individual spikes or large fluctuations in $\Delta F/F$
 409 are observed. However, what can be said for the cells that exhibit a relatively flat and
 410 unchanging profile of fluorescence?

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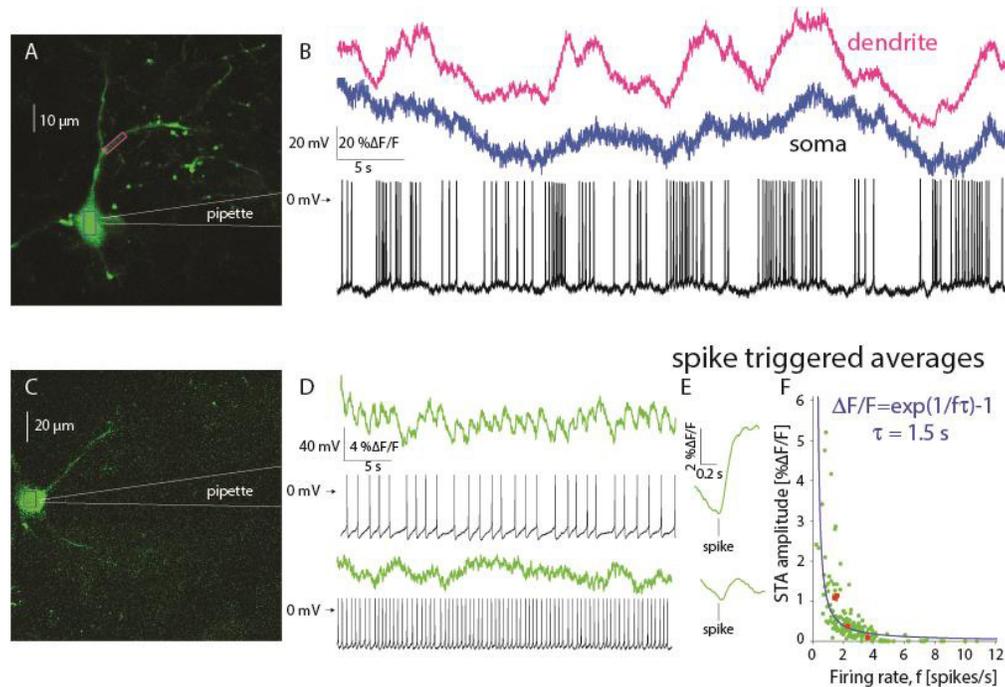


Figure 5. Estimation of autonomous discharge of CINs using 2PLSM GCaMP6 imaging is limited to bursting or to slow regular firing neurons. A. 2PLSM imaging of somatic and dendritic calcium ($\Delta F/F$) signals in conjunction with electrophysiological recording from GCaMP6s-expressing CIN. B. Somatic (blue) and dendritic (pink) $\Delta F/F$ signals and membrane potential of CIN depicted in panel A. C. 2PLSM somatic imaging and electrophysiological recording from another CIN. D. Somatic imaging and corresponding electrophysiological recording from CIN firing autonomously at a lower rate (top) or driven to fire faster at a higher rate (bottom). E. Spike-triggered average (STA) of somatic $\Delta F/F$ signal (from panel D) for slow (top) and fast (bottom) discharge. F. Amplitude of STA vs. the firing rate of regularly firing CINs. Solid blue line: fit of phenomenological model (see text).

411

412 **Limitations in interpreting somatic GCaMP6s signal from autonomously firing CINs**

413 To address this question, we used targeted-patch of CINs in order to characterize
 414 the firing patterns underlying the calcium transients (Figure 5A). We then aligned the trace
 415 from the somatic region of a cell with its corresponding electrophysiological recording.
 416 When a CIN discharged spontaneously in a bursty fashion (Figure 5B, blue), calcium

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417 transients similar to those observed without a patch electrode (Figure 4) were visible, and
418 it was possible to clearly associate the electrophysiological recordings and the large
419 calcium transients. Proximal dendrites exhibited an even clearer relationship to spiking
420 (Figure 5B, pink), due to the larger surface-to-volume ratio (see below). In CINs that fired
421 regularly (Figure 5C), fluorescence transients associated with single action potentials
422 could still be identified, as long as the firing rate was sufficiently low (Figure 5D, top). In
423 this case, estimation of the spike triggered average (STA) of the calcium signal revealed a
424 large $\Delta F/F$ waveform that rose after the action potential occurred and slowly decayed
425 (Figure 5E, top). When the same CIN discharged faster, it was no longer possible to
426 unequivocally discern individual transients (Figure 5D, bottom). Nevertheless, the STA
427 revealed a $\Delta F/F$ waveform that is time-locked to the action potential (Figure 5E, bottom),
428 albeit a significantly smaller one than that observed during slower discharge (Figure 5E,
429 top). This finding suggested the tetanic-like fusing of the individual calcium transients is
430 responsible for the decrease of the STA amplitude. If tetanic fusion of the $\Delta F/F$ signal
431 occurs at firing rates as low as 2-2.5 spikes/s, this effect places strong constraints on the
432 ability to read out the discharge patterns underlying the calcium transients when using
433 GCaMP6s.

434 To quantify this effect, we characterized the relationship between firing rate of the
435 CINs and the amplitude of the STA of the $\Delta F/F$ trace associated with that firing rate. Figure
436 5F depicts a scatter plot of the STA amplitude as a function of firing rate for $n=25$ non-
437 bursting CINs (from $N=15$ mice), where each CIN is represented by at least three points
438 corresponding to different firing rates (e.g., red dots represent 4 measurements from the
439 same CIN). The resulting plot (Figure 5F) shows that the STA calcium transient amplitudes

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440 decrease as the firing rate increases. When the firing rate is too high it becomes impossible
441 to detect the underlying spike times from the fluorescence trace alone, because the average
442 transient is too small to discern against a noisy background. An example for such a case is
443 shown in Figure 5D, bottom, where the neuron fires at ~ 2 -2.5 Hz. Individual action
444 potentials can no longer be discerned from the imaging trace alone even though the
445 estimation of the STA reveals a visible waveform.

446 The dependence of the size of the STA on the firing rate can be captured by a simple
447 phenomenological model (see Materials and Methods) wherein the observed calcium
448 dynamics are simply a sum of the calcium fluorescence transients elicited by the individual
449 action potentials. If we further assume for simplicity that the transient is exponentially
450 shaped (with a decay time constant τ) and that the firing is perfectly periodic, we can
451 derive an expression for the amplitude of the STA as a function of the firing rate that
452 depends on the single parameter τ . The value of τ for the fit (blue line in Figure 5F) is 1.5
453 seconds. The main determinant of this decay is the decay kinetics of GCaMP6s which is on
454 the order of one second (Chen et al., 2013). Additionally, imaging large compartments such
455 as somata further slows the decay kinetics (Goldberg et al., 2009).

456

457 Capacity to detect individual spikes using wide field calcium imaging is diminished

458 From the empirical results and the phenomenological model, it is evident that the
459 faster the neurons fire, the smaller the size of the STA waveform. In other words, the
460 slower the decay kinetics of the indicator the harder it is to discern individual action
461 potentials in the calcium signals. These data demonstrate that the use of GCaMP6s,
462 constrains the ability to detect individual calcium transients if the neuron fires faster than

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463 2-3 spikes/s. But what resolving power is GCaMP6s expected to have under the one-photon
464 conditions employed in the endoscopic imaging? Unlike the sensitivity of 2PLSM imaging,
465 the endoscopic data collected from the awake behaving mouse did not seem to exhibit
466 calcium transients corresponding to individual action potentials. One possibility is that the
467 much slower sampling rate of the endoscope – which smears STAs (Teagarden et al., 2008)
468 – and its low NA (0.5) GRIN lens objective further diminishes the ability to discern
469 individual action potentials. To test this possibility, under more controlled conditions in
470 conjunction with electrophysiological recordings, we conducted wide-field calcium imaging
471 of CINs expressing GCaMP6s in acute slices under conditions that recreate the endoscope’s
472 specification, by using an EM-CCD at a sampling rate of 5-10 Hz via a 20X/0.5 NA objective.

473 The wide-field imaging revealed a diffuse neuropil signal, similar to that seen *in vivo*
474 (Figure 6A). As with the 2PLSM imaging experiments, we were able to discern multiple
475 CINs per slice (Figure 6A), and the calcium transients associated with individual neurons
476 were variable, with some exhibiting large and slow fluctuations while others exhibiting flat
477 traces (Figure 6B). When we combined electrophysiological recordings with the imaging, it
478 was possible to observe gross changes in firing rate in the $\Delta F/F$ signal (Figure 6C).
479 However, when we focused on examples where the discharge was relatively regular, it was
480 impossible to observe fluorescence transients associated with individual spikes.
481 Furthermore, the STAs in these cases were indistinguishable from a flat line ($n=9$ neurons
482 from $N=8$ mice, data not shown).

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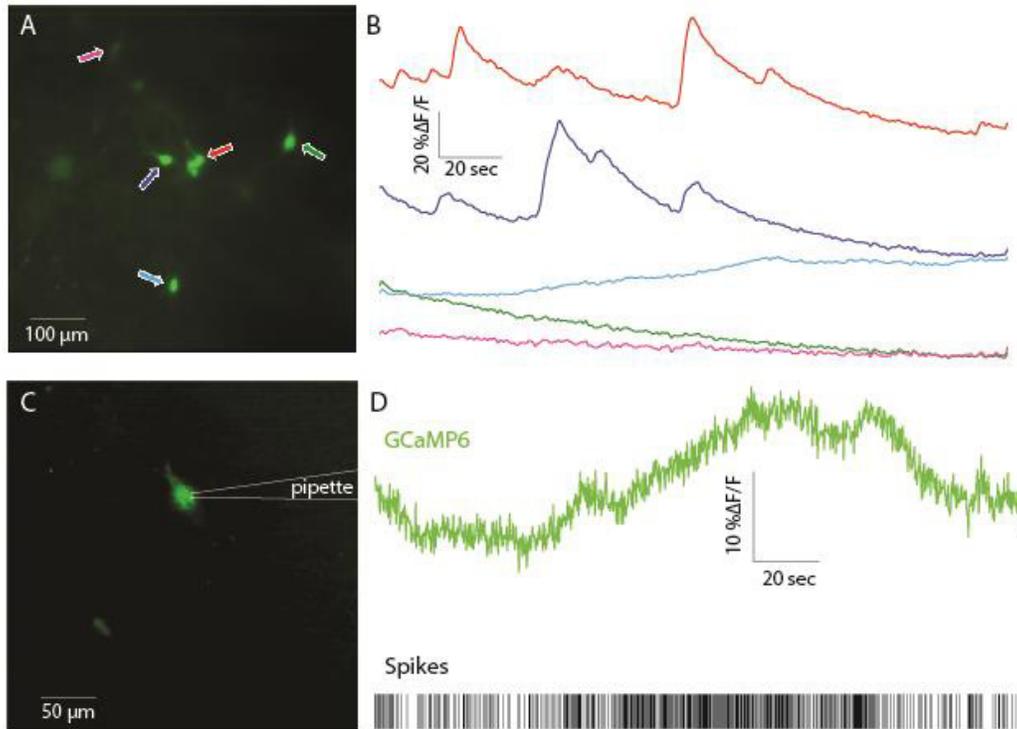


Figure 6. Wide-field one-photon imaging of CIN somata in acute striatal slices. A. Wide-field image of CINs expressing GCaMP6s in an acute striatal slice. Five individual CINs are identified and color coded with arrows. B. Calcium ($\Delta F/F$) signal from the 5 cells depicted in panel A. C. Wide-field image from another cell recorded in cell attached mode. D. Calcium ($\Delta F/F$) in conjunction with spike raster of the CIN depicted in panel C.

483

484 Our conclusion is that a sufficiently slow firing rate is required in order to discern
 485 calcium transients from individual spikes, and that – in our hands – this is achieved reliably
 486 only using 2PLSM. Wide field imaging with a slow camera and a low NA objective will
 487 generate GCaMP6s signals, that follow changes in firing rate, but from which individual
 488 spikes are not detectable. Moreover, when observing a calcium trace with only small
 489 fluctuations it is difficult to determine whether the cell is firing fast or not firing at all. The
 490 conclusion is that with the use of endoscopes one can only observe substantial fluctuations

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491 in firing rate. Moreover, because constant fluorescent signals are usually included in the
492 baseline value (F_0), any relatively regular activity of CINs will generate a basal fluorescence
493 that will be removed when calculating the $\Delta F/F$ signal, and will therefore remain
494 undetected.

495 Origin of the neuropil signal

496 The previous analysis suggests that the fluctuating somatic GCaMP6s signals
497 observed via the endoscope extract only robust changes in the firing rate of CINs. We next
498 turn to consider what neural activity gives rise to the cholinergic neuropil signal observed
499 in endoscopy. Here again we employ 2PLSM in acute striatal slices with GCaMP6s-
500 expressing CINs. As mentioned above, distinct dendritic processes are observed with
501 2PLSM throughout the transfected regions in the striatal slice. As these processes are
502 ubiquitous, and no other cell types express the GECI, we hypothesized that CIN dendrites
503 contribute to the blurred neuropil signal visualized with the endoscopes and the wide field
504 calcium imaging (Figure 1D, movies 1 & 2).

505 Because of the large, global fluctuations of the neuropil signal in the endoscopic
506 imaging, we set out to determine their source. Previous studies of calcium signals in CINs
507 from acute rodent slices using inorganic membrane impermeable dyes (Bennett et al.,
508 2000; Goldberg et al., 2009; Tanimura et al., 2016) demonstrated that bAPs and even long
509 back-propagating subthreshold depolarizations (bSDs), can open dendritic voltage-
510 activated calcium channels (Chen et al., 2013), and generate visible dendritic calcium
511 changes. These are certainly candidate mechanisms to generate dendritic GCaMP6s signals.
512 However, because the neuropil signal preceded the somatic signals in the endoscopic data,
513 we considered another possibility, that activation of afferent glutamatergic inputs could

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514 introduce sufficient calcium influx via NMDA and calcium permeable AMPA receptors, both
515 of which are expressed in CINs (Consolo et al., 1996; Kosillo et al., 2016; Aceves Buendia et
516 al., 2017), to generate a visible calcium signal. In order to determine which of these three
517 scenarios – namely bAPs, bSDs or activation of ionotropic glutamate receptors – is
518 responsible for the dendritic signals, we compared the size of the GCaMP6s $\Delta F/F$ signals
519 generated by each of these physiological processes.

520

521 Back-propagating action potentials are a major contributor to the neuropil signal

522 To determine whether bAPs or bSDs are the main contributors to the dendritic
523 calcium signal, we target-patched CINs, silenced them with a hyperpolarizing holding
524 current, and injected sub- or supra-threshold depolarization currents while measuring the
525 resulting calcium transient at a proximal dendrite. Comparison of the size of the transients
526 evoked by back-propagating sub- and supra-threshold depolarization revealed that bAPs
527 generated a significantly larger calcium signal in dendrites, that were quantified by the
528 integrated fluorescence beneath the $\Delta F/F$ curve for a period of 800 ms (median bAP
529 integrated fluorescence: 0.6875, median bSD integrated fluorescence: 0.048, $P = 7.8 \times 10^{-3}$,
530 SRT, data not shown). This result suggests that of the first two possibilities, bAPs are the
531 main source of the GCaMP6s neuropil signal, whereas the contribution of sub-threshold
532 calcium entry is negligible.

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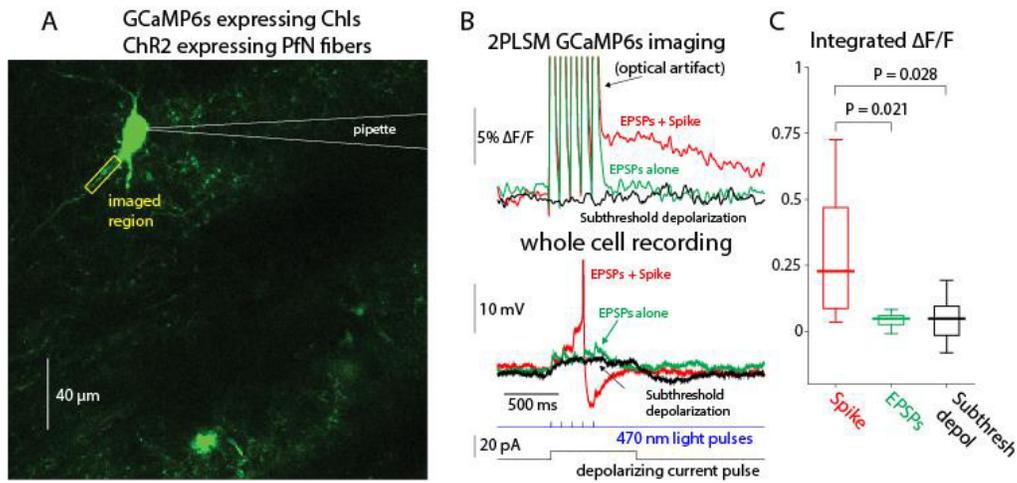


Figure 7. Dendritic GCaMP6 signals detectable using 2PLSM imaging are limited to back propagating action potentials (bAPs). A. 2PLSM imaging of somatic and dendritic calcium ($\Delta F/F$) signals in conjunction with electrophysiological recording from GCaMP6s-expressing CIN surrounded by parafascicular nucleus (Pfn) fibers expressing ChR2 (not shown). B. Calcium ($\Delta F/F$) signals in response to optogenetic activation of Pfn synapses elicits either a subthreshold (green) or suprathreshold (red) synaptic response (bottom) in CIN depicted in panel A. Only the spiking response elicits a detectable $\Delta F/F$ signal. Subthreshold depolarization (in another cell) does not elicit a detectable response (compare to Goldberg et al. 2009). C. Distribution of integrated $\Delta F/F$ response in response to spontaneous bAPs, subthreshold EPSPs and subthreshold depolarization.

533

534 In order to test whether synchronous activation of glutamatergic inputs could also
 535 generate visible calcium transients in CIN dendrites, we injected mice with AAVs harboring
 536 channelrhodopsin-2 (ChR2) with a ubiquitous promoter into the thalamic parafascicular
 537 nucleus (Pfn), which gives rise to the dominant glutamatergic input to CINs (Lapper and
 538 Bolam, 1992; Ding et al., 2010; Threlfell et al., 2012; Aceves Buendia et al., 2017). Thus, in
 539 acute slices from these animals, CINs expressed GCaMP6s while thalamic fibers expressed
 540 ChR2. Two-to-three weeks after transfection, we target-patched CINs (Figure 7A) and
 541 evoked excitatory synaptic potentials (EPSPs) in the patched CIN using full-field 470 nm
 542 LED illumination (Figure 7B). We compared the integrated dendritic calcium signal in

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543 response to sub-threshold EPSPs to the dendritic calcium signal generated by
 544 spontaneously occurring bAPs in the same cells. The calcium transient generated by
 545 spontaneous bAPs was significantly larger than the transient that corresponded to the sub-
 546 threshold EPSPs (Figure 7C, median bAP transient integrated fluorescence: 0.2803, median
 547 EPSP transient integrated fluorescence: 0.0382, $P = 0.0195^c$, SRT. The values for
 548 subthreshold current pulses are shown, as well, for comparison).

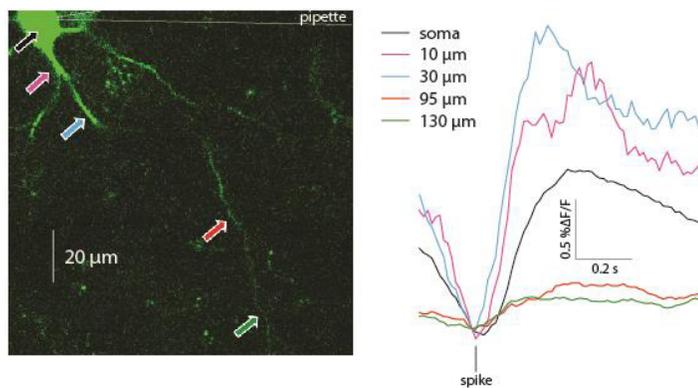


Figure 8. Spike triggered averages of calcium transients elicited by bAPs at various distances from the soma. 2PLSM line scans performed at various linear distances from the soma of a GCaMP6s expressing CIN.

549 Because the slice is filled with many fluorescent processes it was only possible to
 550 reliably identify the proximal dendrites belonging to the patch-clamped CIN. Thus, strictly
 551 speaking the previous analysis relates to calcium transients in proximal dendrites.
 552 Nevertheless, it was occasionally possible to observe bAPs infiltrating distal regions, up to
 553 150 μm from the soma (Figure 8), as reported previously (Tanimura et al., 2016). We
 554 conclude that only bAPs generate a visible dendritic calcium signal. Indeed, as expected
 555 from surface-to-volume ratio considerations, and as has been shown previously with
 556 inorganic calcium indicators (Bennett et al., 2000; Goldberg et al., 2009) the ongoing
 557 GCaMP6s $\Delta F/F$ fluctuations are significantly larger in the dendrites than in the soma

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558 (Figure 5A), as observed by comparing STAs of dendritic transients to STAs of somatic
 559 transients ($n=23$ cells from $N=13$ mice, $P = 7.35 \times 10^{-4}$, SRT)(Figure 9).

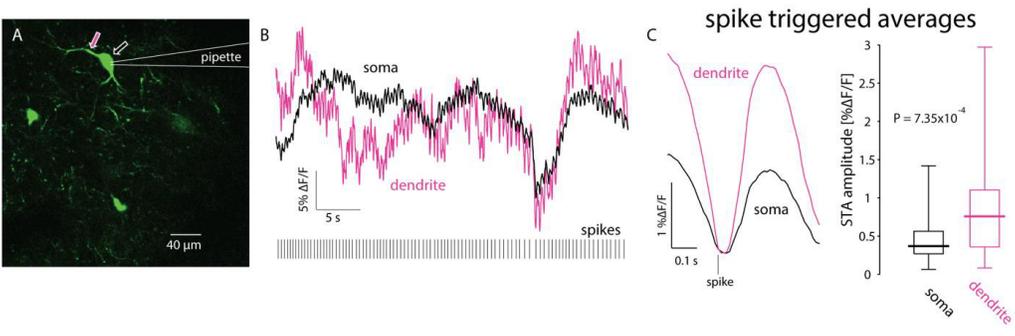


Figure 9. Dendritic calcium transients are larger than somatic ones. A. 2PLSM imaging of somatic and dendritic calcium ($\Delta F/F$) signals in conjunction with electrophysiological recording from GCaMP6s-expressing CIN. B. Calcium ($\Delta F/F$) responses in soma (black) and proximal dendrite (pink) during spontaneous discharge (bottom). C. STA of proximal dendritic (pink) calcium signals is larger than the somatic (black) signal. Right: paired comparison of the amplitude of somatic and dendritic STAs.

560

561 **The neuropil signal represents a mean-field readout of the entire CIN network**

562 In light of the above experiments, it is likely that the background activity seen in the
 563 endoscopic *in vivo* imaging results from bAPs arising from CINs scattered throughout the
 564 striatum whose somata may not be visible but whose dendrites are within the FoV. While
 565 axons are not readily visible in these experiments (Bennett et al., 2000; Goldberg et al.,
 566 2009), we cannot rule out the APs propagating along the CINs' axonal arbors also
 567 contribute to the background activity. Whenever a GCaMP-expressing CIN fires, its entire
 568 dendritic (and possibly axonal) arbor lights up. Because the axonal and dendritic arbors of
 569 CINs overlap and cover the whole striatum (Chang et al., 1982; DiFiglia, 1987; Wilson et al.,
 570 1990; Kawaguchi, 1992), a pixel whose depth of field is tens of microns integrates the
 571 fluorescent signals of bAPs from dendrites of many neurons. Nearby pixels will integrate

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572 similar signals and will therefore be highly correlated. Because this correlated signal is the
 573 sum of the activity of many cells it represents a “global mode” of CINs activity. Because the
 574 global mode arises from the bAPs in CINs, it can be considered a read-out of the “mean-
 575 field” of the recurrent network activity of the entire CINs population.

576 If the neuropil signal is a mean-field readout of the recurrent CIN network, then it is
 577 clear why on average the peak of the somatic signals coincides with the peak of the
 578 neuropil signal. What then gives rise to the 2 second rise in the population response that
 579 precedes the peak response of individual CIN soma? The most likely explanation is that the
 580 population (neuropil) signal represents the gradual recruitment of many CINs.
 581 Consequently, it is slower to rise than the signal from each individual neuron (as seen in
 582 the somatic signals). Additionally, when sampling a single neuron from a large population
 583 that is being recruited, it is expected that the onset of the signal from the single neurons
 584 will follow the population average. This is particularly true in our case where we sample
 585 neurons that are on the dorsal surface of the striatum, and where it is likely that the
 586 activation begins in the more ventral bulk of the striatum. We therefore conclude that the
 587 neuropil signal represents bursts of concurrent neuronal discharge of the striatal
 588 cholinergic network as a whole. This signal can be considered a mean-field cholinergic
 589 signal that is complementary to the signal recorded from individual CINs. Future work is
 590 necessary to determine the behavioral correlates of this signal.

	Data Structure	Type of Test	Power
a	Ranks	Two-tailed Wilcoxon signed-rank test for paired replicates	3.7×10^{-4}

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b	Ranks	Two-tailed Wilcoxon signed-rank test for paired replicates	7.8×10^{-3}
c	Ranks	Two-tailed Wilcoxon signed-rank test for paired replicates	0.0195
d	Ranks	Two-tailed Wilcoxon signed-rank test for paired replicates	7.35×10^{-4}
Table 1. Statistical Table			

591

592 **Discussion**

593 The combination of GECIs and microendoscopic imaging provides an exciting
594 opportunity for studying the collective dynamics of striatal CINs in freely moving animals.
595 CINs are autonomously active (Bennett and Wilson, 1999; Surmeier et al., 2005) and have
596 extensive axonal and dendritic arbors (Chang et al., 1982; DiFiglia, 1987; Wilson et al.,
597 1990; Kawaguchi, 1992). These properties generate a significant neuropil calcium signal.
598 Our investigation of this signal uncovered synchronous patterns of activation in striatal
599 cholinergic neuropil. Our analysis suggests that bAPs are major contributors to the neural
600 activity giving rise to the background signal seen in endoscopy. Finally, we show that the
601 neuropil signal acts as an order parameter representing the striatal CIN network as whole
602 and is, in this sense, similar to LFP.

603 Performing endoscopic calcium imaging of pacemaking neurons raises several
604 issues that require careful consideration. First, the proper method of analyzing calcium
605 signals using $\Delta F/F$ as a proxy for changes in calcium concentrations does not allow the
606 detection of baseline spiking activity exhibited by regularly firing pacemakers. We
607 combined calcium imaging and slice electrophysiology to demonstrate that 2PLSM calcium
608 imaging using GCaMP6s only reveals individual spikes in pacemakers if their discharge rate
609 is sufficiently low (~ 2 spikes/s). This is due to the relatively long decay time constant of

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610 GCaMP6s (Chen et al., 2013) that does not allow for the sufficient decay of calcium signals
611 between consecutive spikes. Somatic calcium dynamics may introduce an additional delay,
612 further hindering the detection of single action potentials. In the case of endoscopic
613 imaging, the low sampling rate and low NA associated with miniaturized endoscopes add a
614 major constraint, which makes it difficult to detect individual spikes even with averaging.
615 Nevertheless, endoscopic calcium imaging has critical advantages over electrophysiological
616 recordings - in particular, the ability to detect spatial patterns in the activity of a
617 molecularly identified neural population.

618 We exploited this advantage to demonstrate a temporal structure in the recruitment
619 of striatal cholinergic neuropil. The temporal recruitment is manifested in the earlier rise of
620 the integrated neuropil signal compared to the somatic signals of individual neurons.

621

622 Our results suggest that the background neuropil signal seen in endoscopic *in vivo*
623 calcium imaging arises primarily from the integrated fluorescent signal of bAPs from many
624 CINs dispersed throughout the striatum (we cannot entirely rule out that subthreshold or
625 synaptically driven calcium influx contribute to the signal, but their contribution is
626 negligible in comparison to suprathreshold calcium influx). The fact that the decay time of
627 the neuropil signal is shorter than that of the somatic signals (Figure 3C), supports the
628 interpretation that it arises primarily from dendrites (and/or axons) because their surface-
629 to-volume ratio is higher. The higher ratio speeds up the decay constant of the axodendritic
630 fluorescent signals relative to somatic ones (Goldberg et al., 2009). Thus, the cholinergic
631 neuropil signal acts as a mean-field readout of the recurrent activity of the network of
632 striatal CINs. This is reminiscent of the LFP signal – a once neglected signal that is now

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633 extensively studied and believed to represent integrated synaptic activity (Creutzfeldt et
634 al., 1966; Eggermont and Smith, 1995; Bedard et al., 2004; Goldberg et al., 2004). We show
635 that fluctuations in neuropil fluorescence are, like fluctuations in the LFP signal (Eckhorn
636 and Obermueller, 1993; Destexhe et al., 1999), highly correlated in space. In addition,
637 somatic calcium events are preceded by neuropil calcium events. This again resembles the
638 LFP signal, which coincides with increases in instantaneous firing rate (Lass, 1968;
639 Donoghue et al., 1998; Destexhe et al., 1999). Thus, the background neuropil signal is a
640 signal with physiological significance.

641

642

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795 **Multimedia legends**

Movie 1. Synchronous spatiotemporal patterns in striatal cholinergic neuropil of a freely moving mouse. Microendoscopic imaging of the DLS of a freely-moving mouse expressing the calcium indicator GCaMP6s selectively in CINs. The size of the visualized area is approximately 600 μm by 900 μm , and the movie is presented in real time. Imaging reveals fluctuations in the fluorescence of cholinergic neuropil characterized by rapid bursts of activation that permeate the entire field of view and decay slowly. The movie includes three examples of activation events.

Movie 2. The cholinergic neuropil calcium signal precedes the somatic signal. Surface plot visualization of the microendoscopic calcium imaging signal in the DLS of a freely-moving mouse (as in Movie 1). Visualized area is a 40 μm by 60 μm patch consisting of a single CIN soma surrounded by cholinergic neuropil. Example of an activation event demonstrating that somatic fluctuations are superimposed upon the temporal fluctuations of surrounding pixels and are slightly preceded by them.

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